



Master in Electrical and Electronics Engineering

EE-517: Bio-Nano-Chip Design

Lecture #5

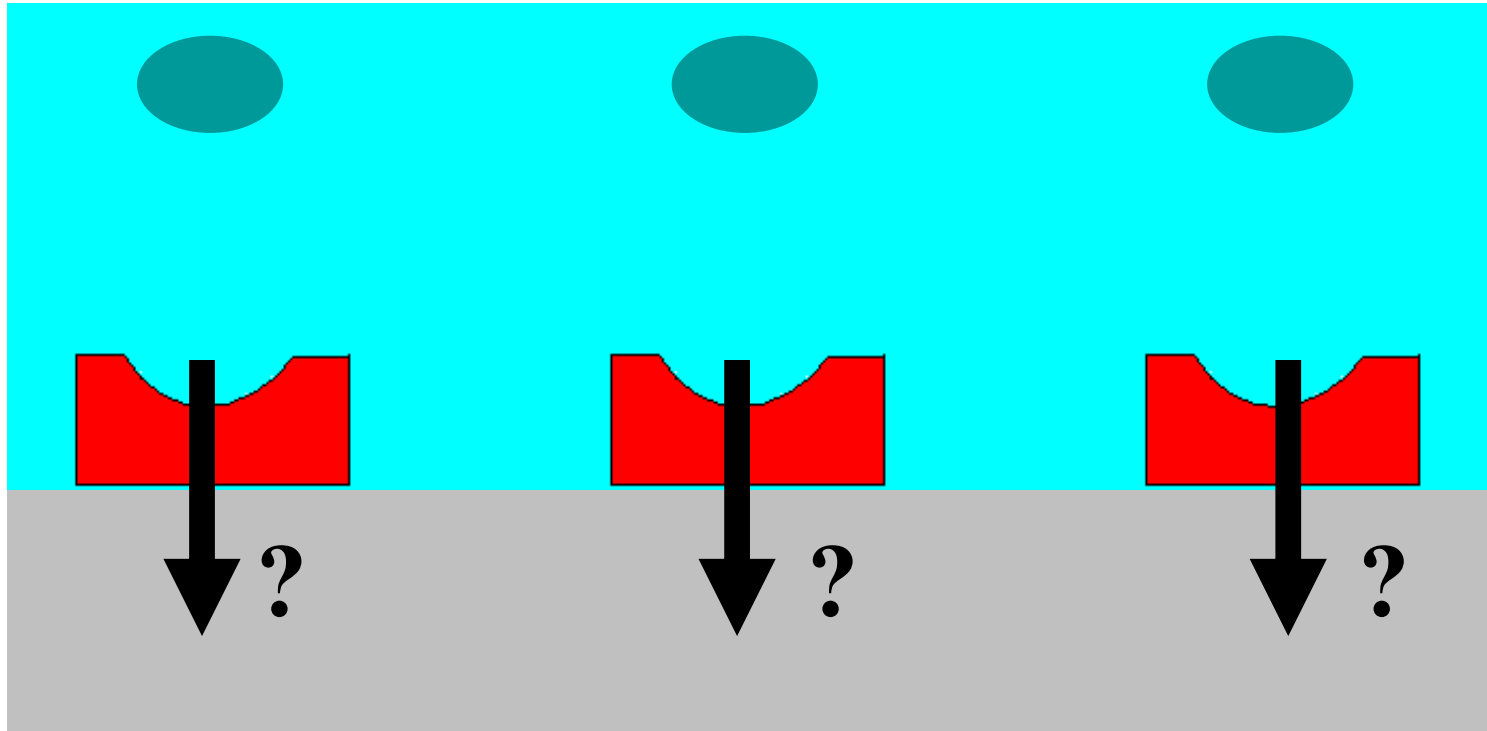
Probe Detection Principles (with Antibodies and DNA)

Lecture Outline

(Book Bio/CMOS: Chapter' paragraphs § 6.1-4 & 6.8)

- Uptake Ab/Ag @ Bio/CMOS interface
- DNA hybridization @ Bio/CMOS
- Layering effects with DNA or Antibodies
- Helmholtz Planes & Debye Length

CMOS/Sample sensing interface



The interface between the CMOS circuit and the bio-sample needs to be deeply investigated and organized



Q1

Do the antibodies always target the same epitope in the antigens?

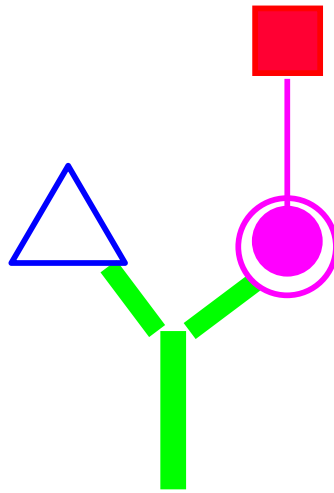
- A. Yes, of course!
- B. May be, depending on the type of antibodies
- C. No, only in case of very simple antigens
- D. Never: each antibody targets a different epitope

Different Kinds of Antibody

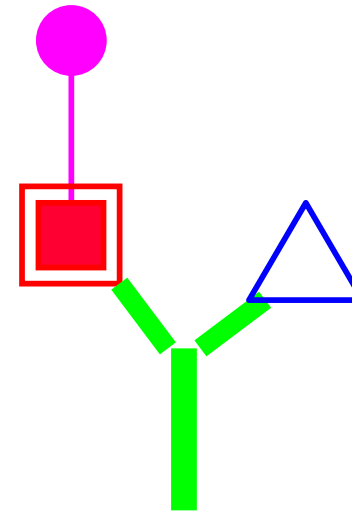
Dealing with real cases results in a bit more complex situation than just adding antigens to antibodies with a unique perfect match. Monoclonal antibodies are, then, all antibodies that have exactly the same specificity because they are from the same cloned single cell. However, antibodies are in general secreted in blood plasma by cells that are from different cell lines. Therefore, it is easy to obtain antibodies that are all against the same antigen but that do not have exactly the same specificity: these are polyclonal antibodies. Different kinds of antibodies means different kinetics on the same antigen.

We may also obtain different kinetics by involving the same antibody. It happens when the secreted antibody possesses two different paratopes to address two different epitopes of the same antigen

Polyclonal Antibodies



Antibody 1



Antibody 2

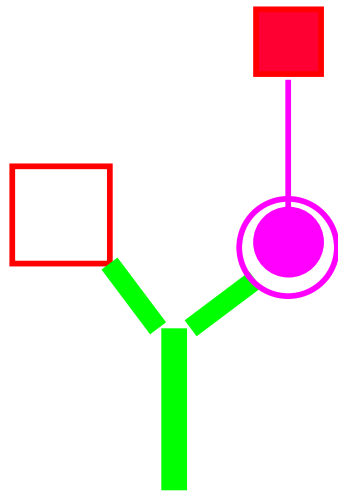


Q2

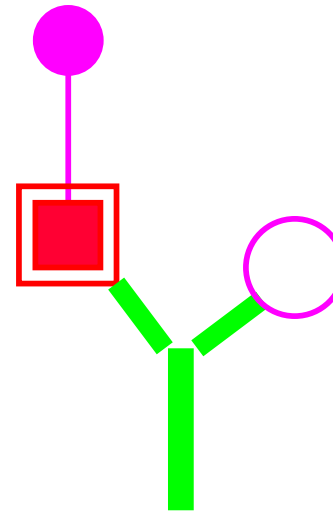
May the same antibody targets two different antigen' epitopes?

- A. Yes, of course!
- B. No, only in case of very complex antigens
- C. May be, depending on the type of antibodies
- D. Never: each antibody targets only an epitope

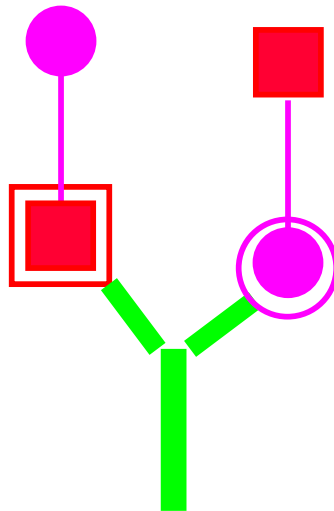
Different monomers with same antibody



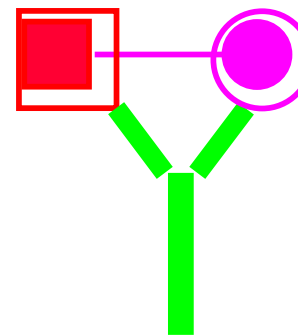
Simple Monomer



Simple Monomer

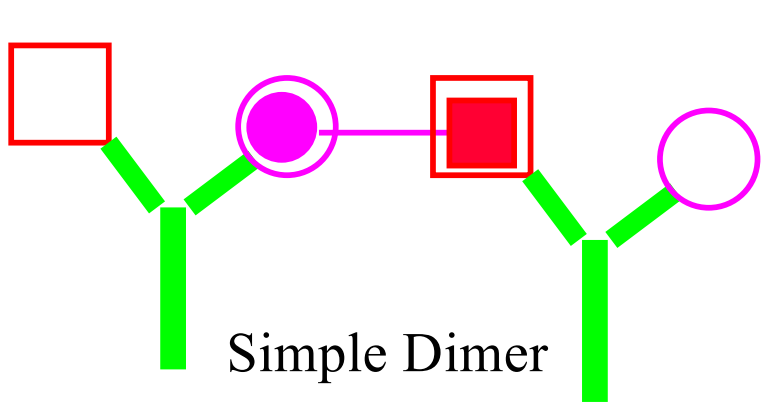


Fully-Saturated Monomer

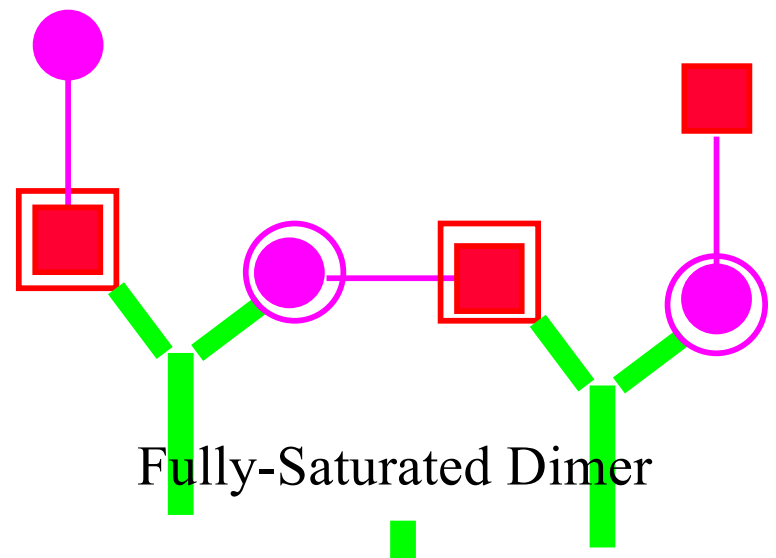


Closed Monomer

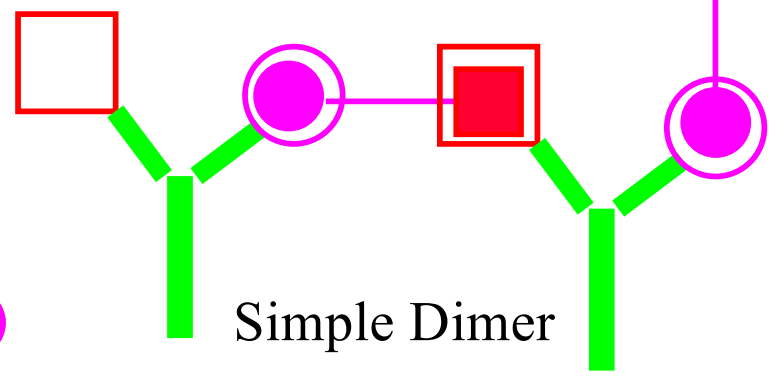
Different dimers with two antibodies



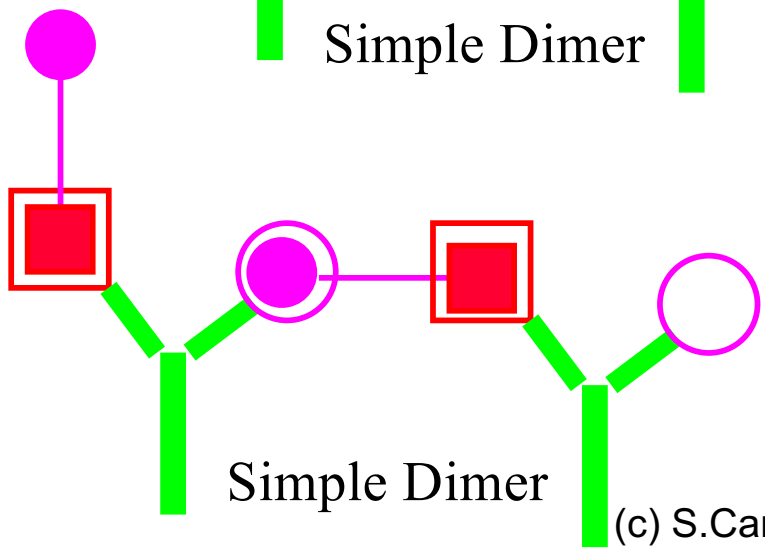
Simple Dimer



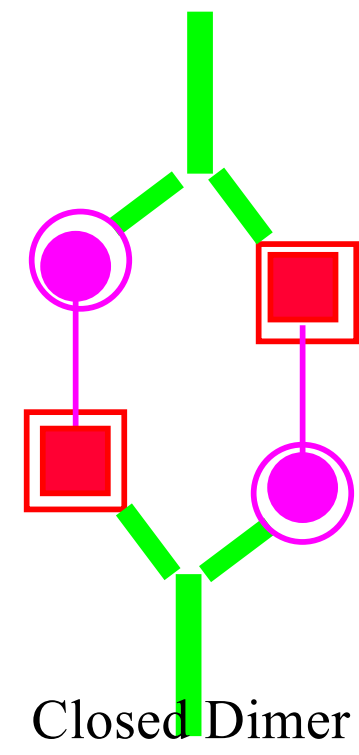
Fully-Saturated Dimer



Simple Dimer



Simple Dimer



Closed Dimer

(c) S.Carrara

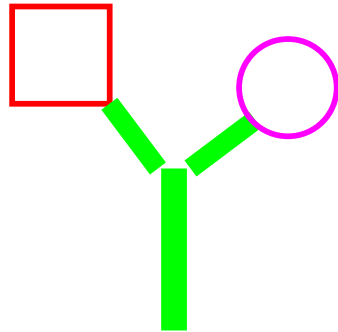


Q3

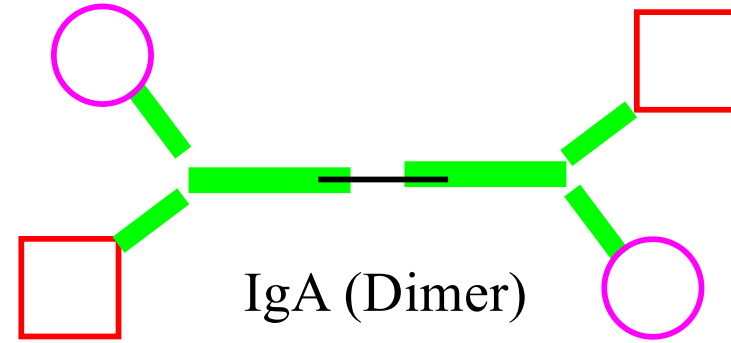
Do antibody exist only in Y-shape?

- A. Yes, of course!
- B. Not in the case of very complex antibodies
- C. May be, depending on the type of antibodies
- D. Never: all antibodies are differently-shaped

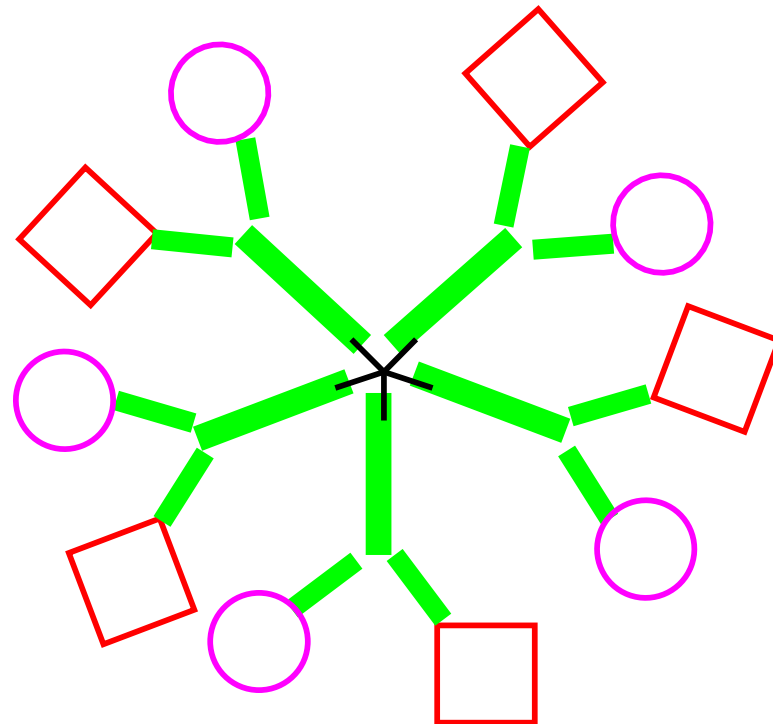
All possible classes of immunoglobulins



IgG, IgE, and IgD (Monomer)

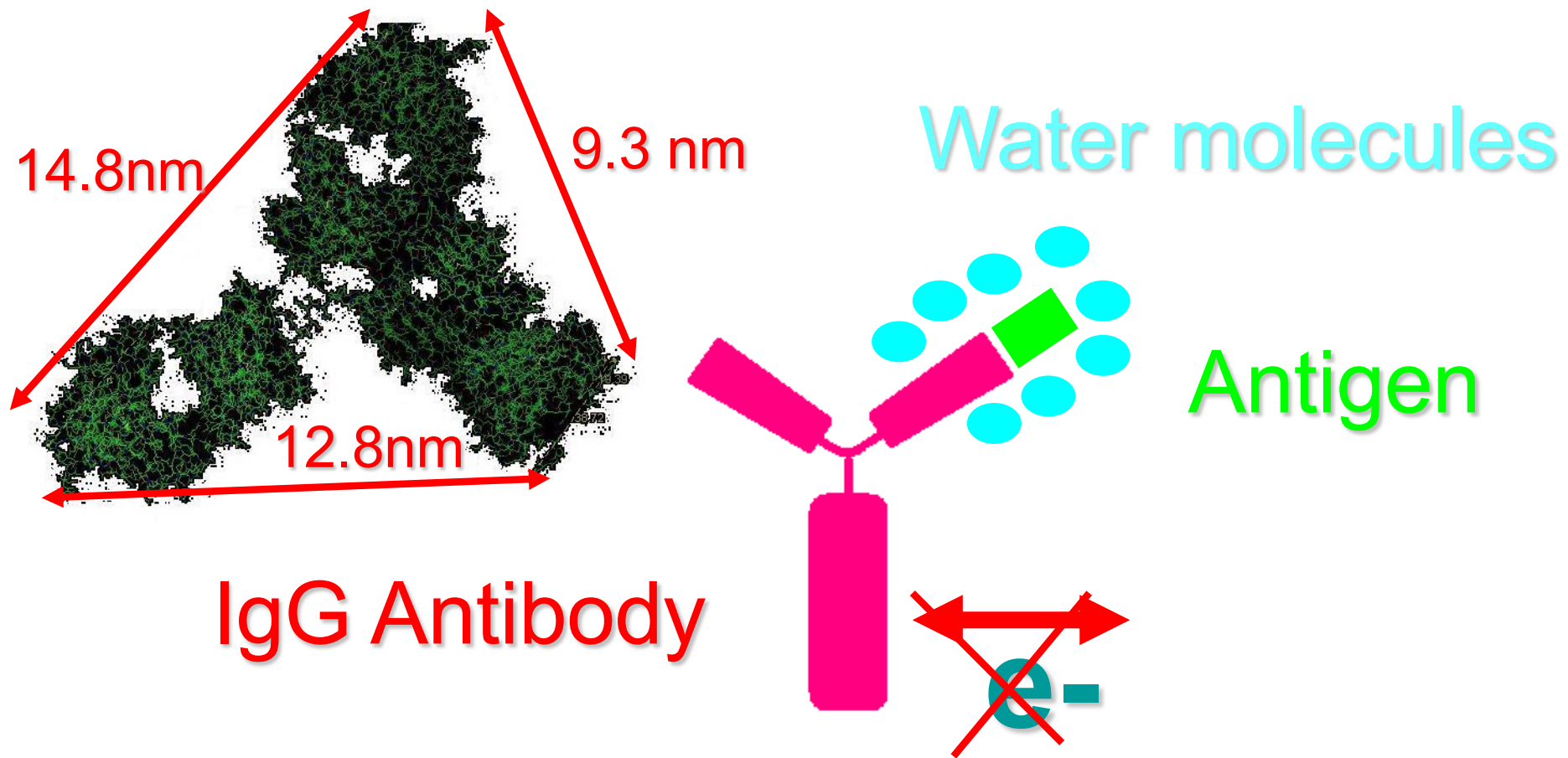


IgA (Dimer)



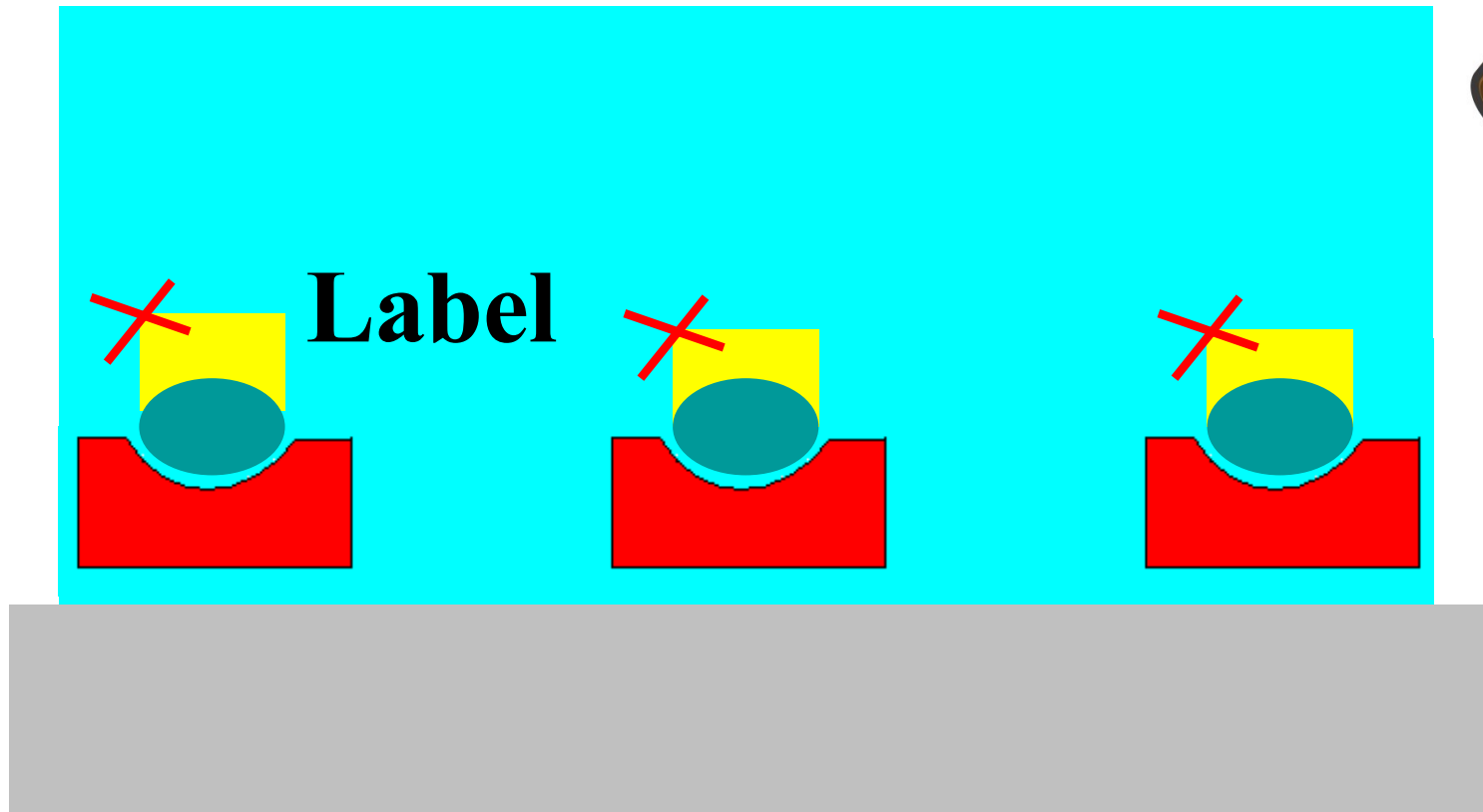
IgM (Pentamer)

The interaction Ab/Ag



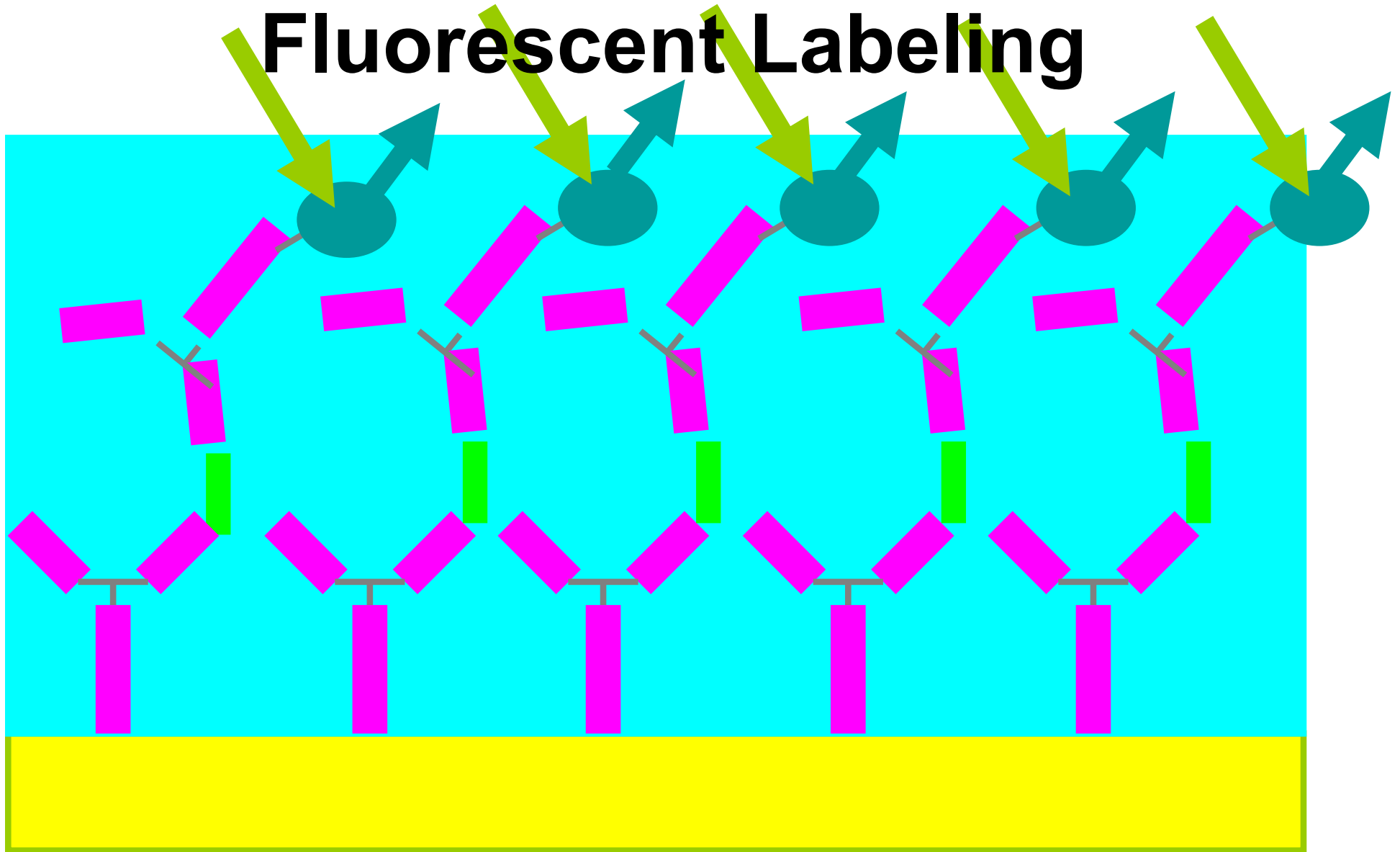
The antigen rests in a very tight binding pocket which is exactly the right size and shape to receive it. Other important factors include enthalpic contributions from van der Waals interactions and hydrogen bonds, and entropic contributions from the release of bound water upon antigen binding

Measuring Bio-Markers



The Measure of Bio-markers may be performed in a labeled manner or in label-free mode

Fluorescent Labeling



Antigens are specific detected by Secondary Antibodies with Fluorescent Labels

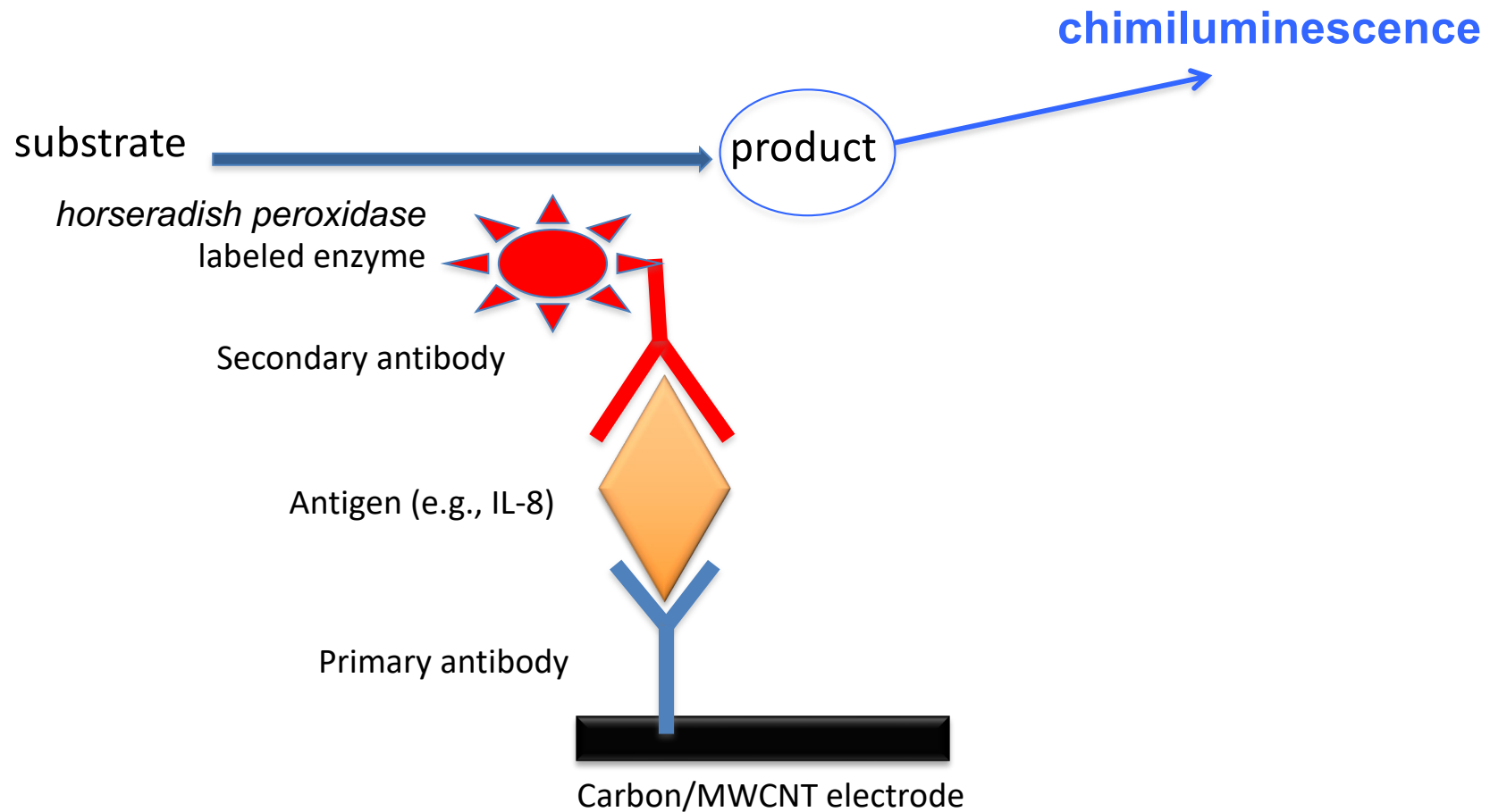


Q4

Is the fluorescence label the only possible label?

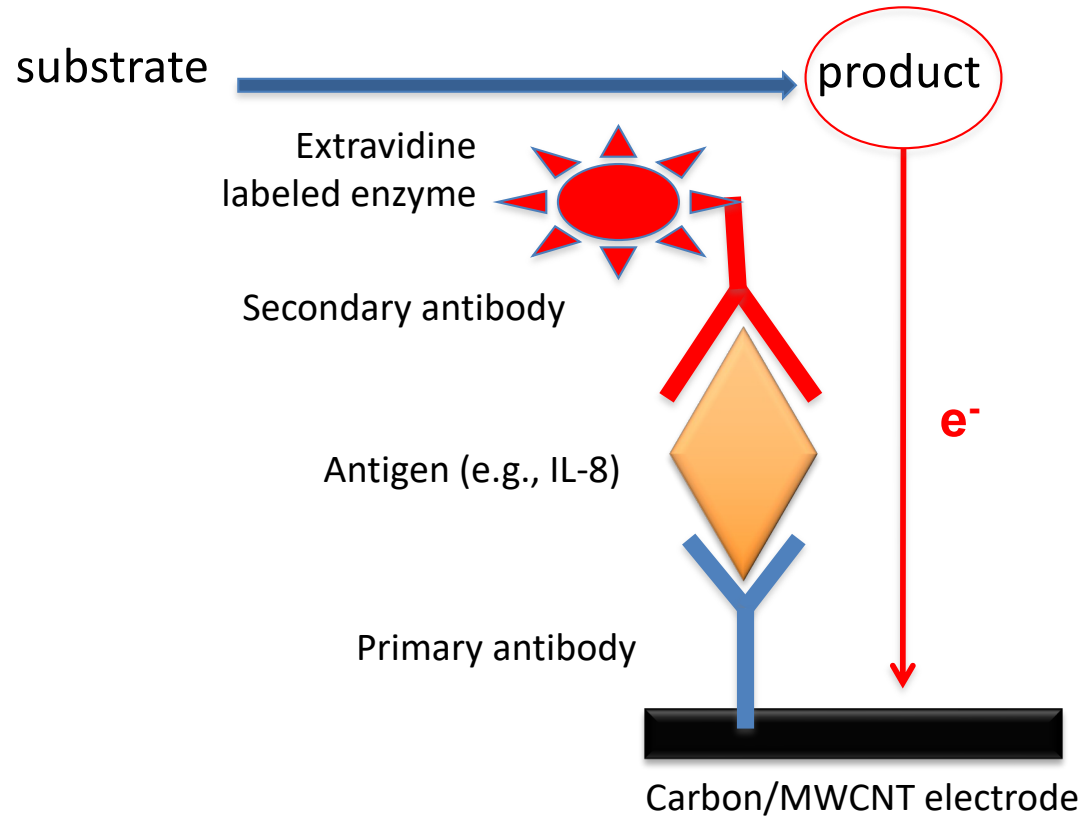
- A. Yes, of course!
- B. No, depending on the type of antibodies
- C. No, depending on the type of antigens
- D. Not at all**

Chemiluminescence Labeling



Antigens are specific detected by Secondary Antibodies with Chemiluminescence Labels

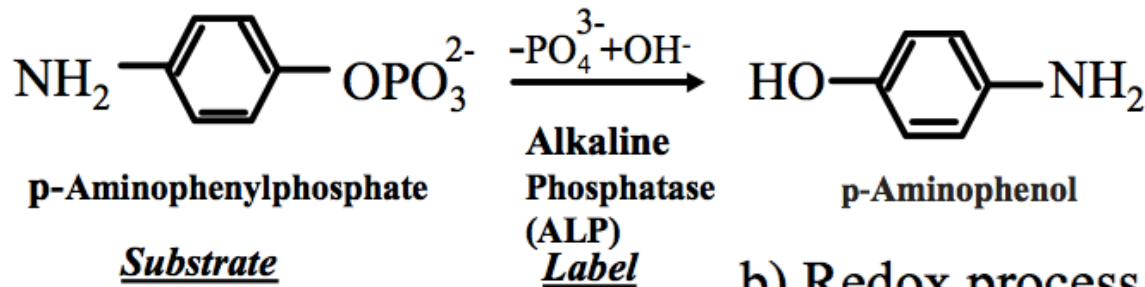
Electrochemical Labeling



Antigens are specific detected by Secondary Antibodies with Electrochemical Labels

Electrochemical Labels

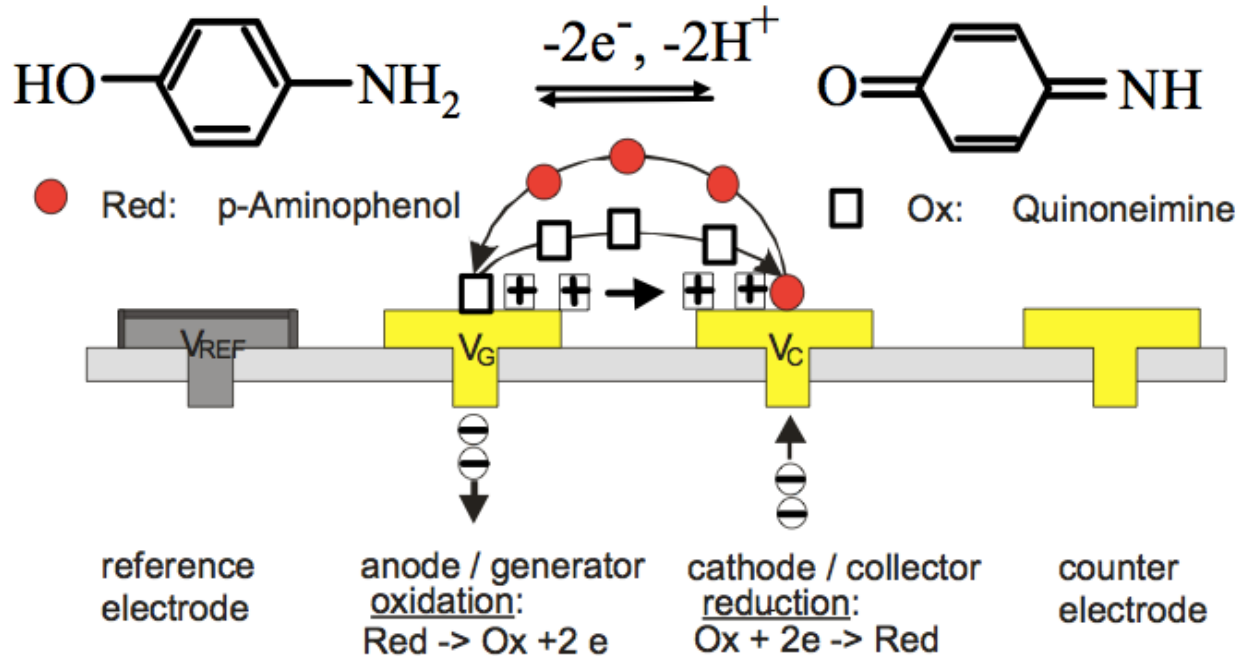
a) Process at the label



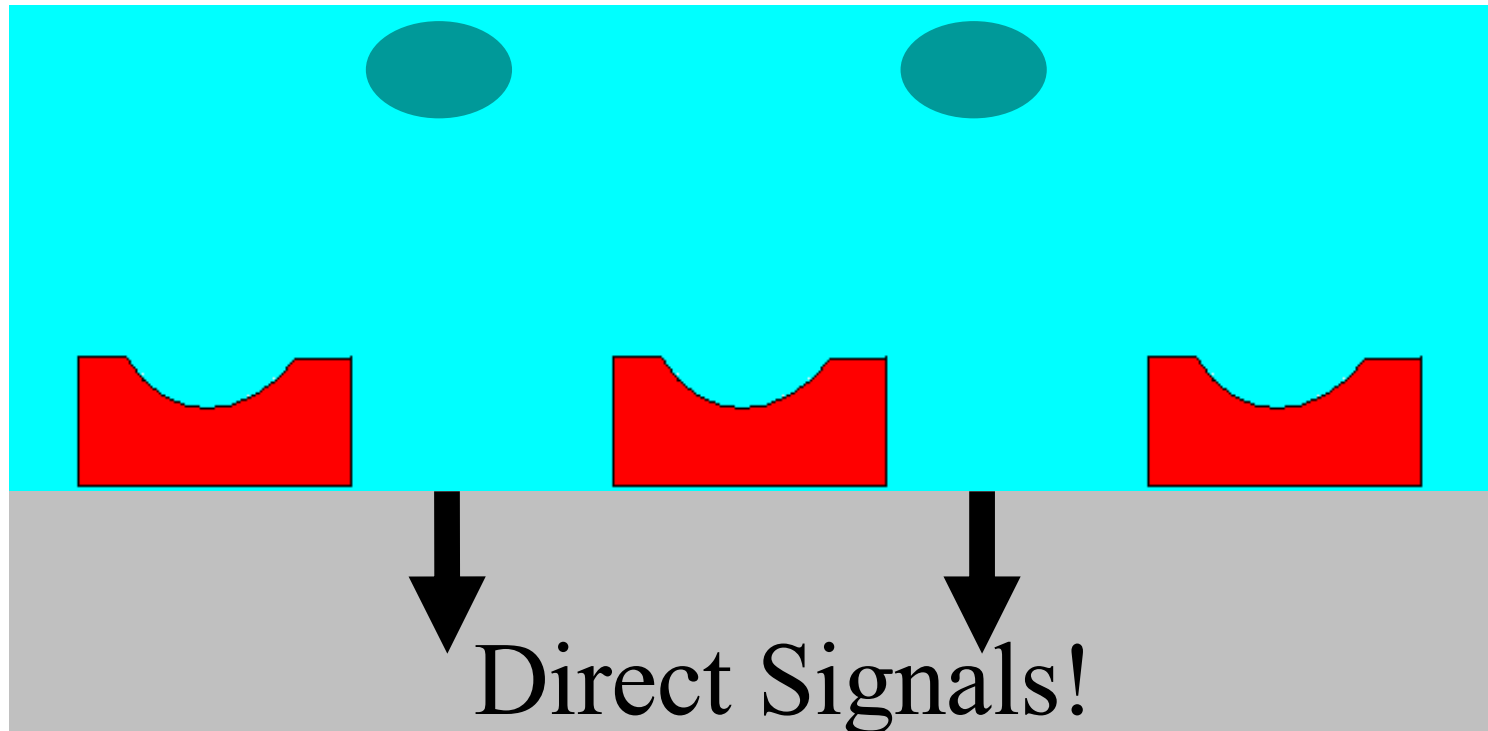
✓ The label cleaves the secondary probe

✓ The product of the cleavage is generating an oxidation process at the anode and, once oxidized, a reduction at the cathode

b) Redox process at the electrodes

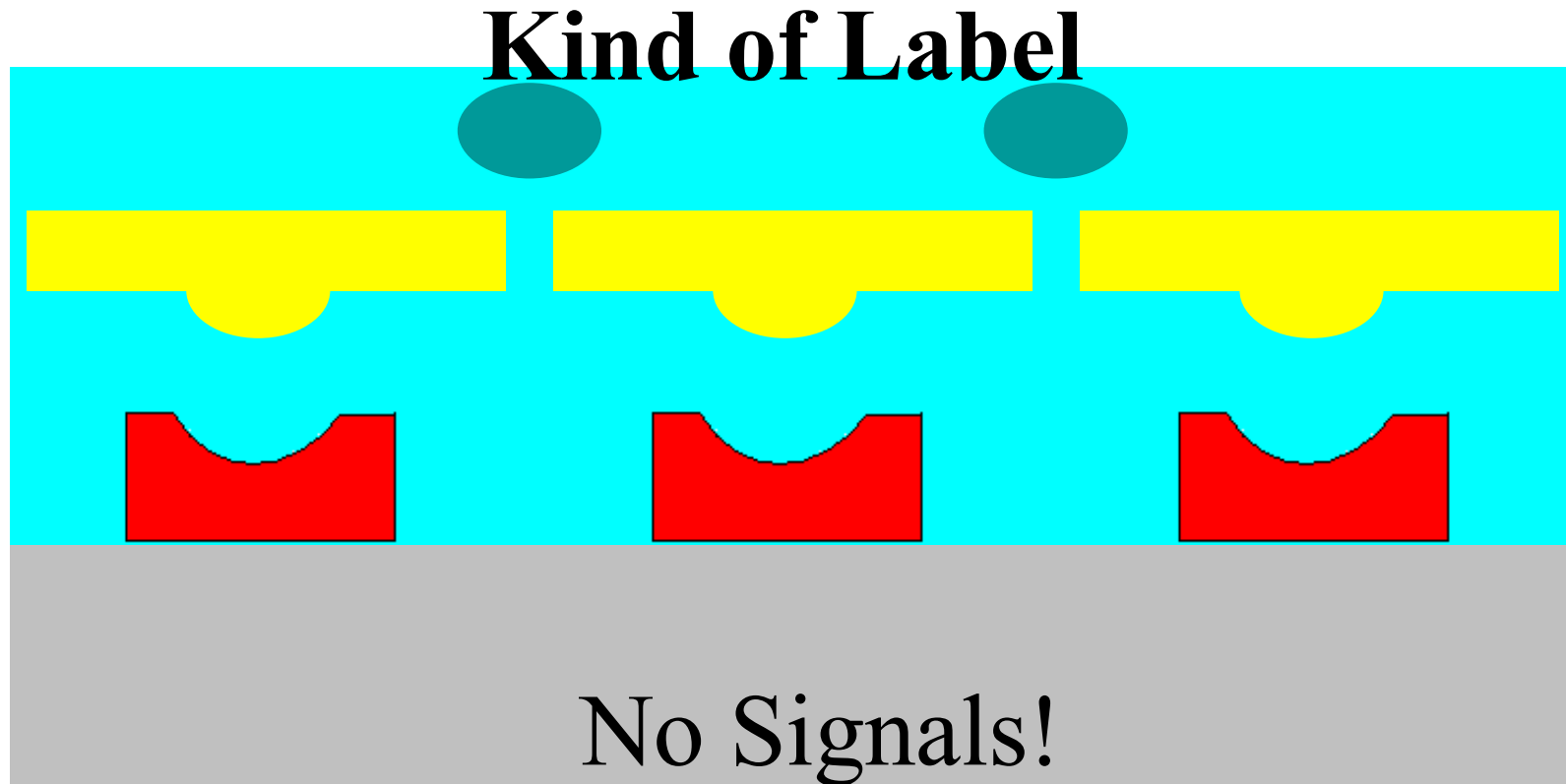


CMOS/Sample interface



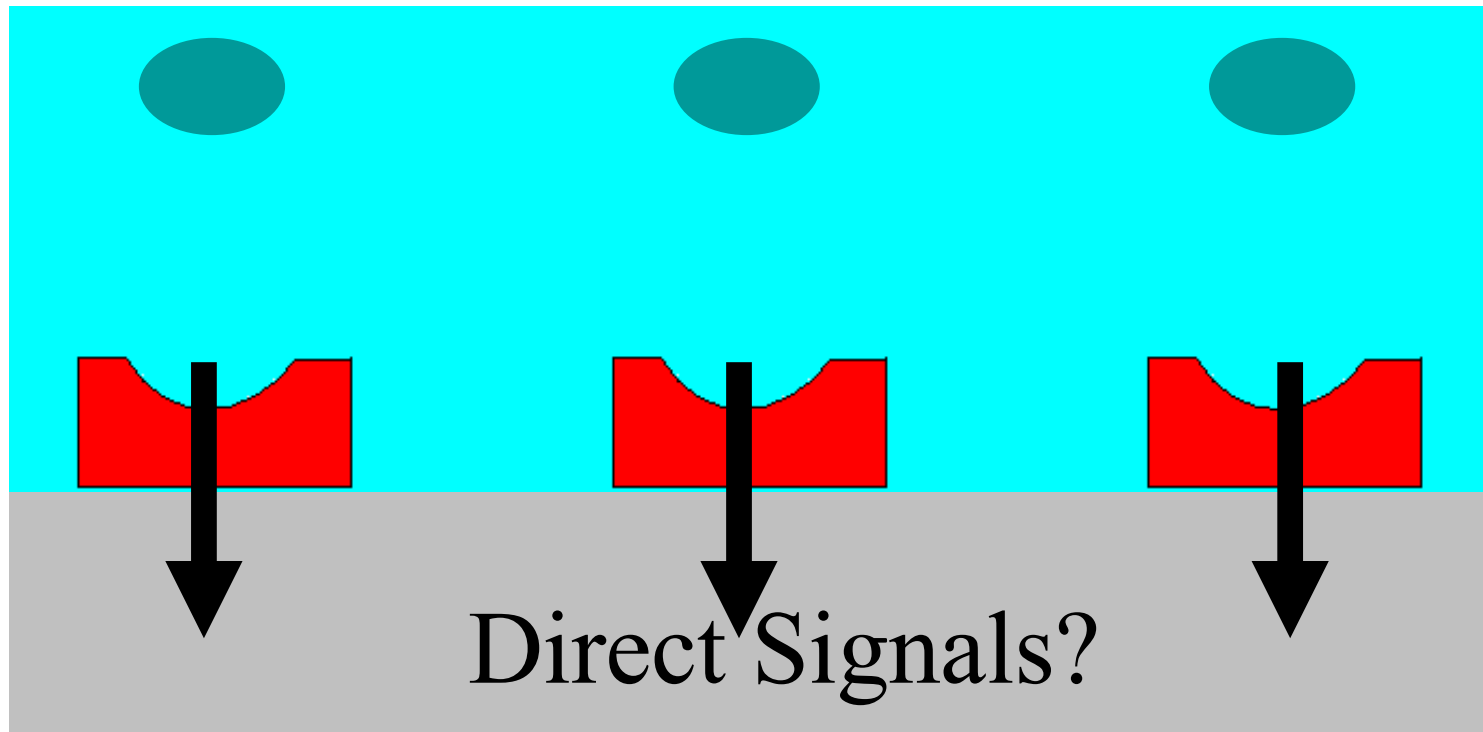
How to get direct signals of probe/target interactions?

CMOS/Sample interface



How to get direct signals of probe/target interactions?

CMOS/Sample interface



How to get direct signals of probe/target interactions?



Q5

Any chance to get direct electrical signals from Ab/Ag interaction?

- A. No, of course!
- B. Yes, depending on the type of antibodies
- C. Yes, depending on the type of antigens
- D. Yes, looking for changes in potential
- E. Yes, looking for changes in surface' charge



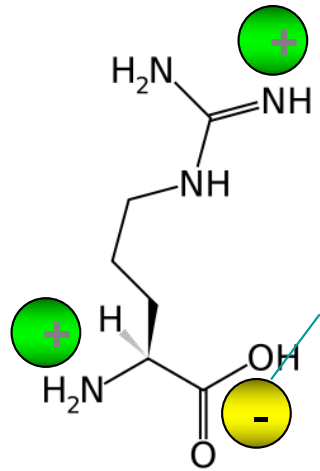
Q6

Any charge on amino-acid residues?

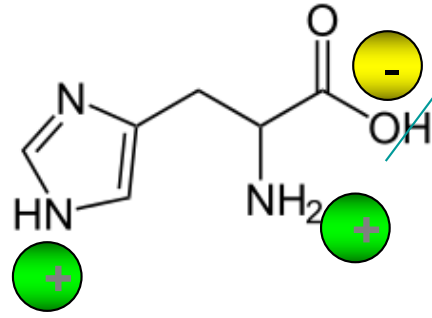
- A. No: all are neutral molecules!
- B. No especially if they are kept in physiological conditions
- C. Always, once they are kept in physiological conditions
- D. Some, once they are kept in physiological conditions

Charged Residues

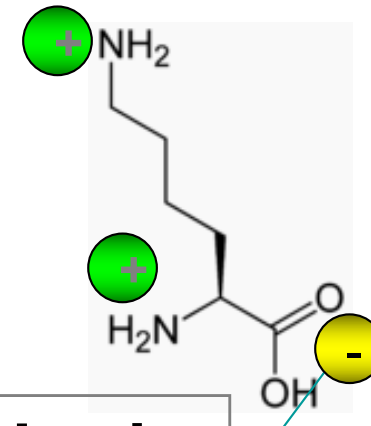
Positively Charged



Arginine

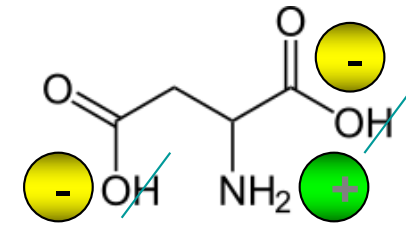


Histidine

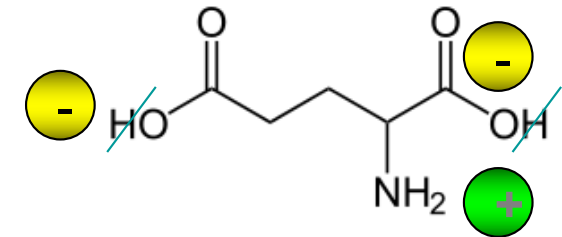


Lysine

Neg. Charged

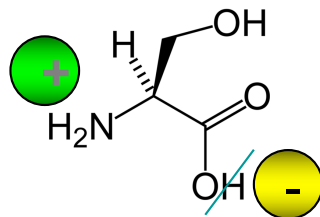


Aspartic Acid

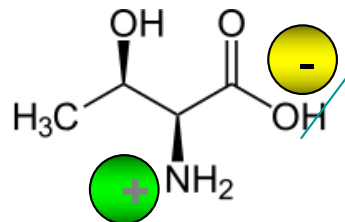


Glutamic Acid

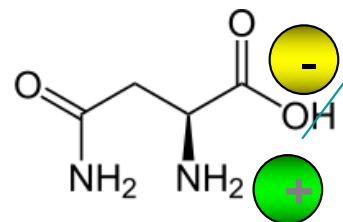
Polar Uncharged



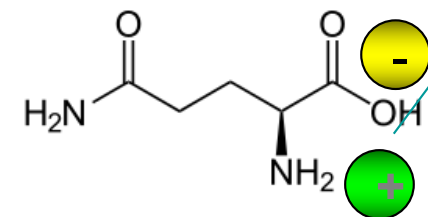
Serine



Threonine



Asparagine



Glutamine



Q7

Any net charge on Ab once they are kept in physiological conditions?

- A. No, all are neutral molecules!
- B. No, since their positive/negative residues compensate
- C. Yes, since their positive/negative residues do not compensate
- D. Yes, since they have only positive or negative residues

The charges of an Antibody



The crystallographic structure of an antibody

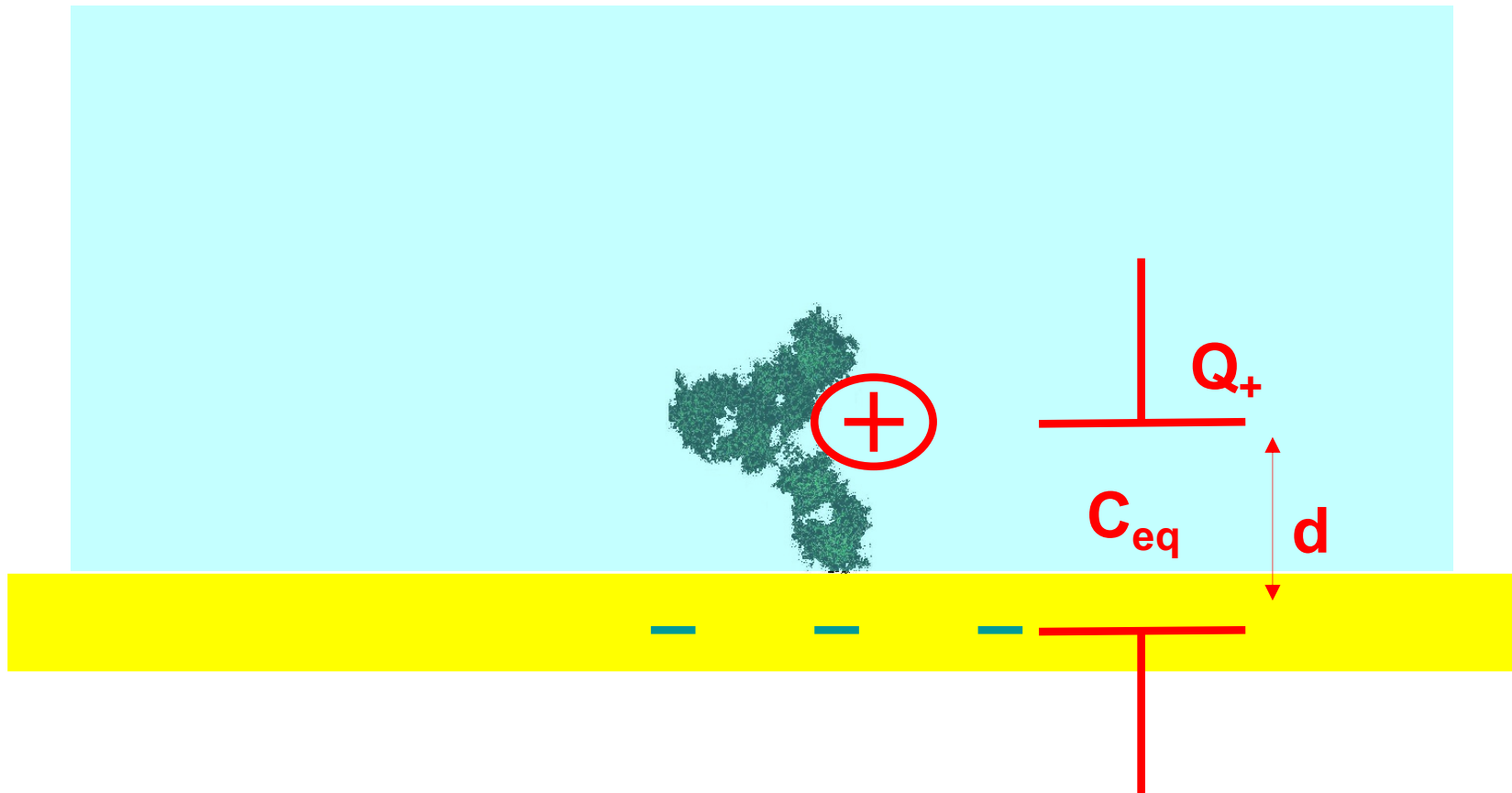


Q8

How I can measure the net charge of an Ab?

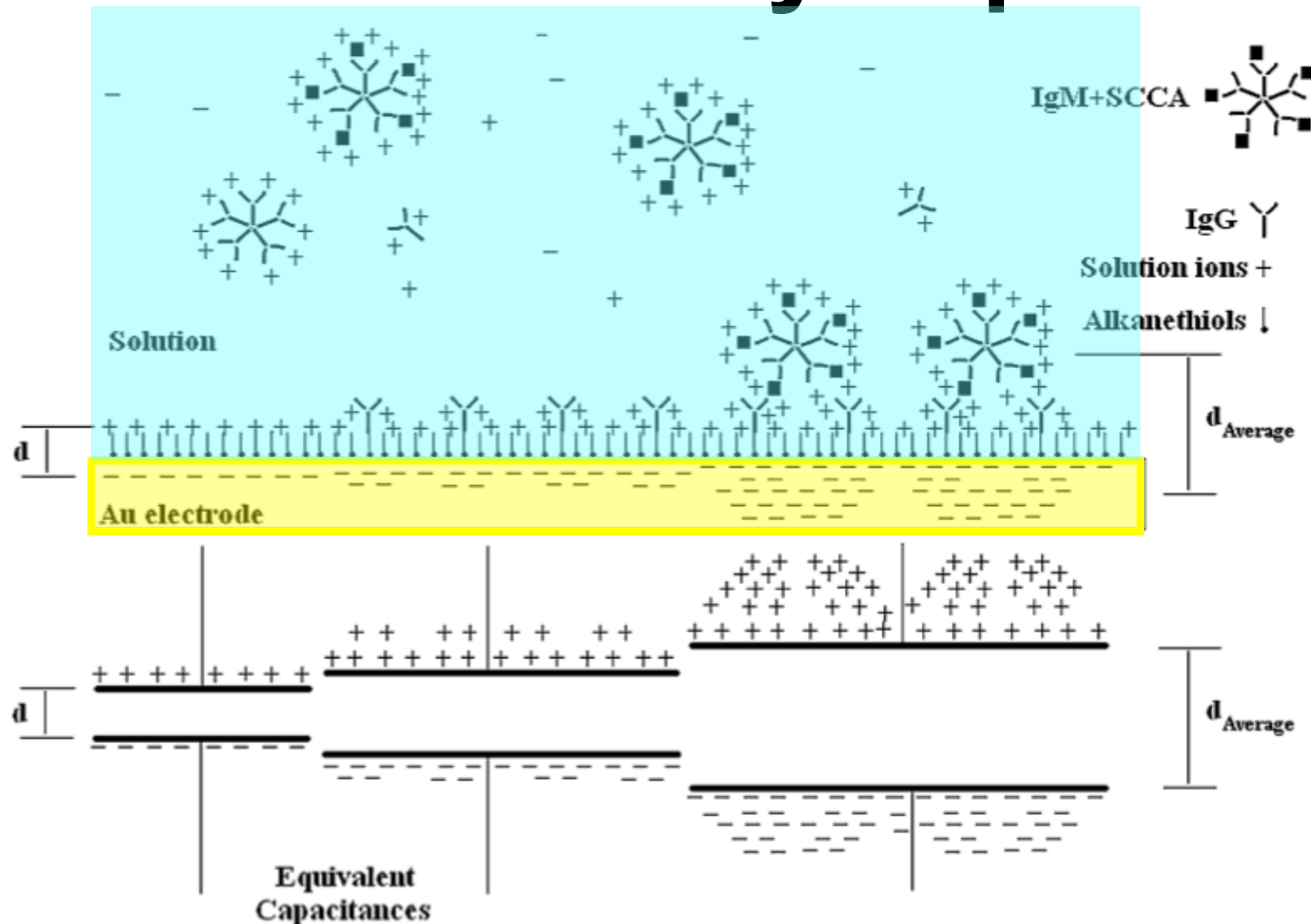
- A. With a measure of a current
- B. With a measure of a potential
- C. With a measure of a capacitance
- D. With a measure of a resistance
- E. With a measure of an inductance

Capacitive detection



Charged residues of the antibody may affect charge carriers in the electrode

Cancer Detection by capacitance



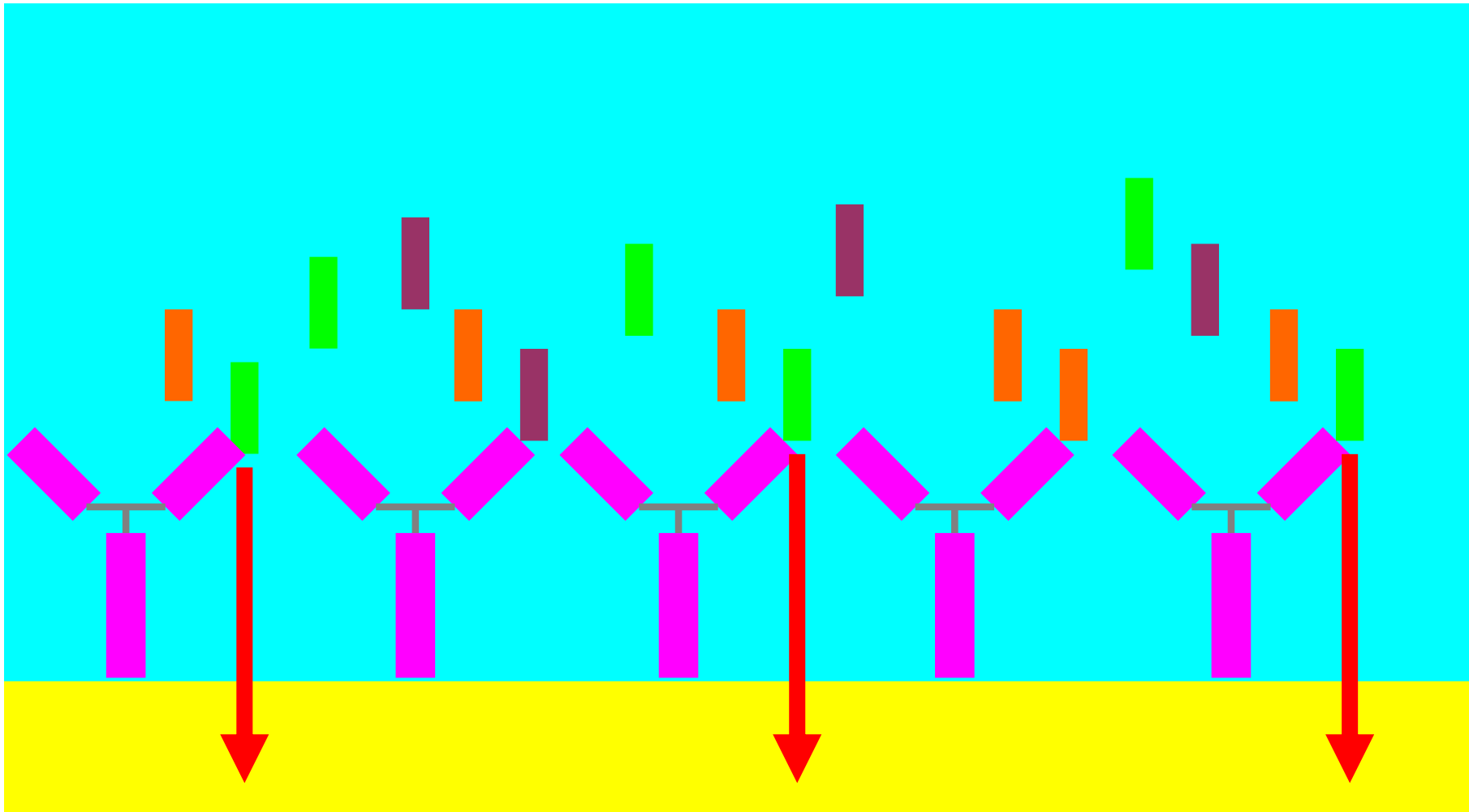
Schematic of the capacitive detection principle

Problem of Specificity



Find your friend in a very crowded square!

Specificity of the Probe



Antigens are specific detected by immobilizing the right antibodies

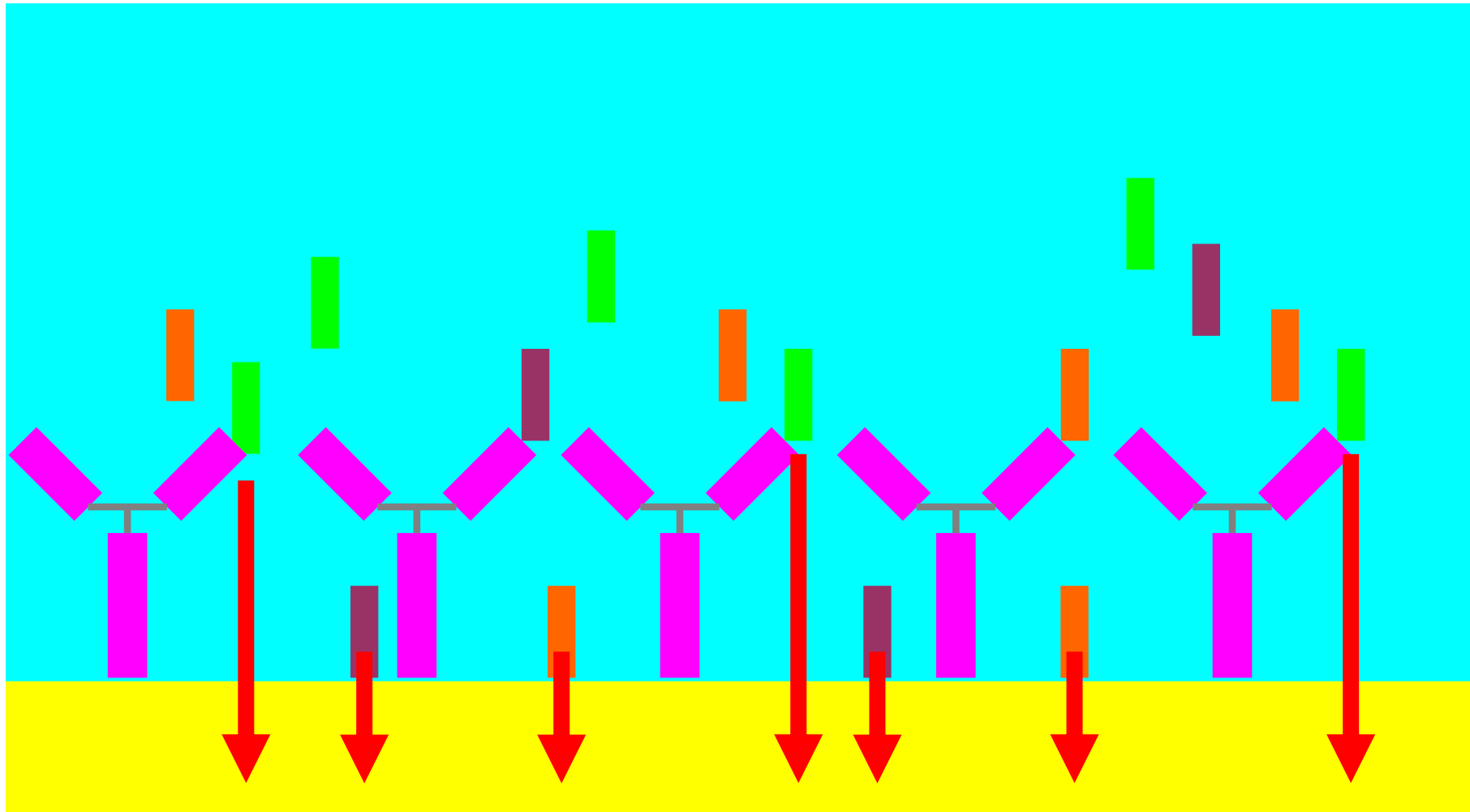


Q9

May I think to have a very-specific Ag detection once got a very-specific Ab?

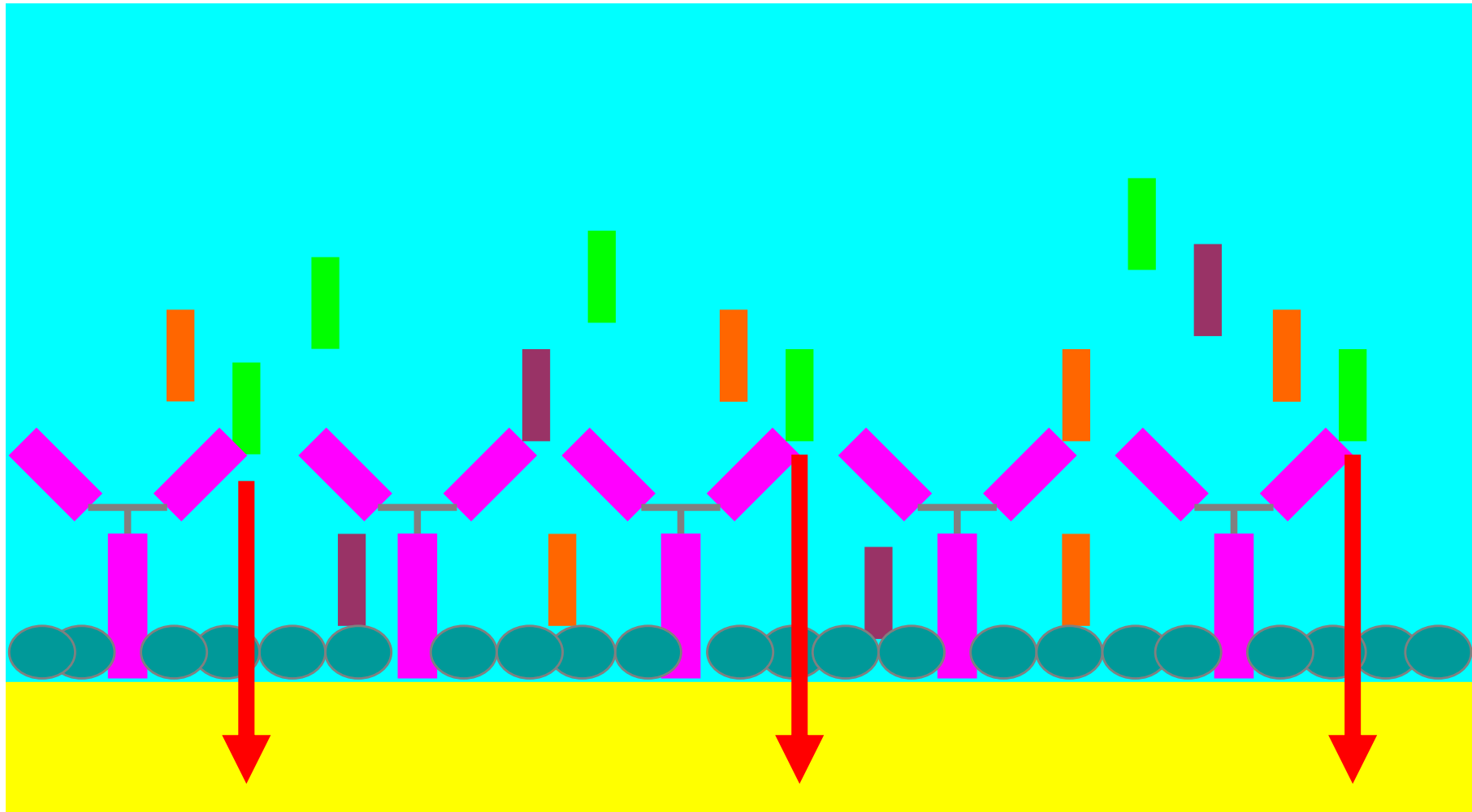
- A. Yes, of course!
- B. Yes, but only in case of monoclonal antibodies
- C. May be, depending on the kind of antibody
- D. May be, depending on the kind of antigen
- E. No at all**

Specificity of the Surface



Antibody are specific but the resulting surface might not be specific enough

Specificity of the Surface



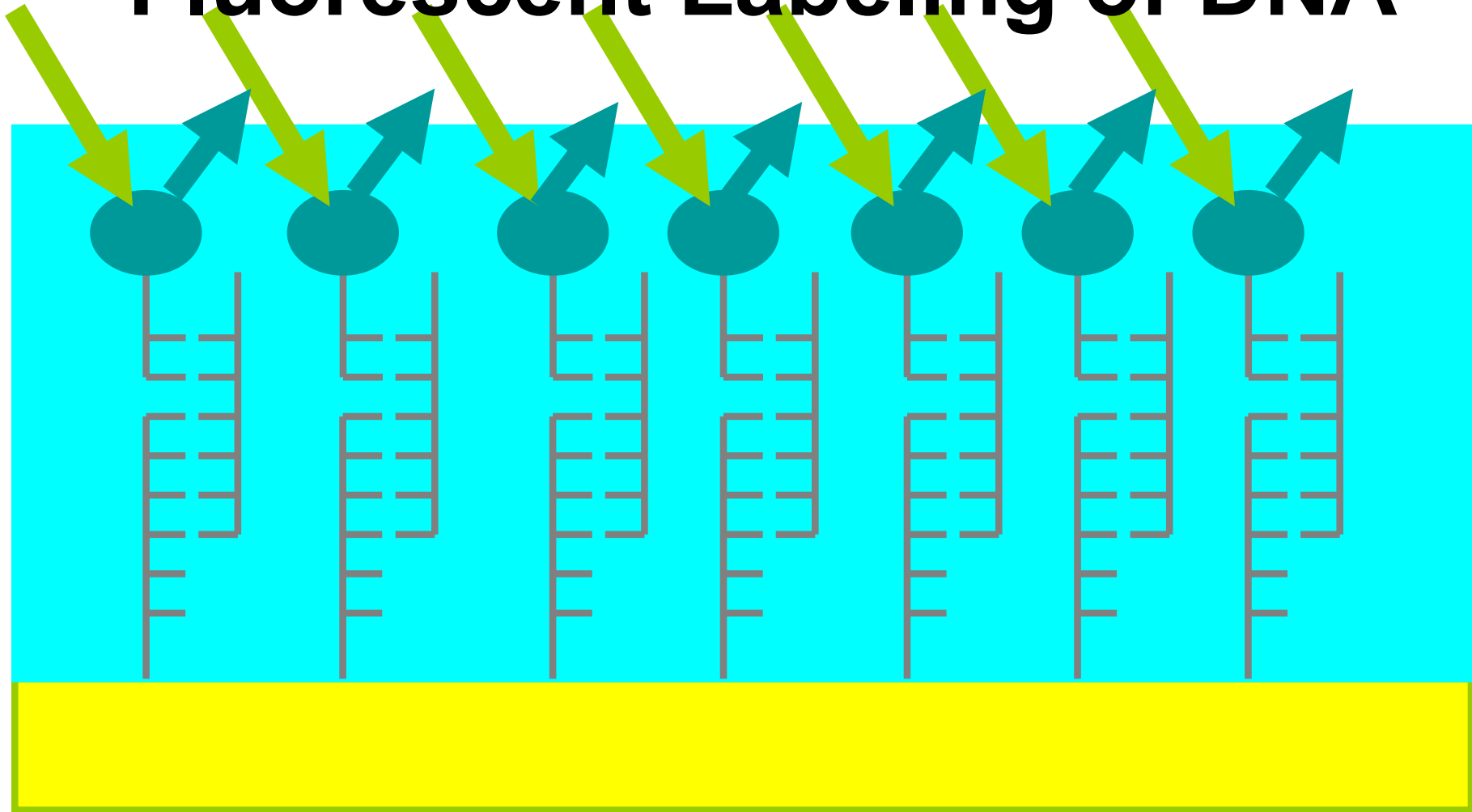
Blocking agents are used
to improve surface specificity

Specificity of the Probe

Duplex	ΔG [kJ/mol]
GGTTATTGG CCAATAACC	-26.8
GGTTATTGG CCAAAACC	-12.0
GGTTCTTGG CCAATAACC	-12.4

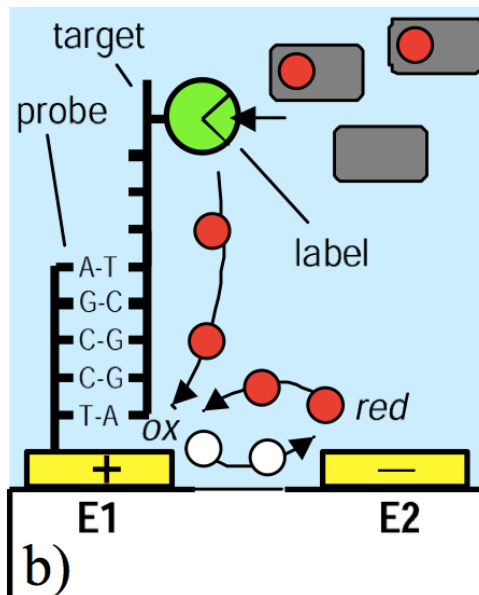
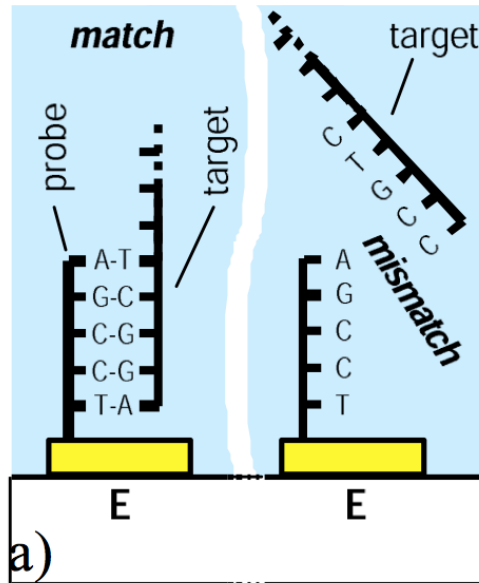
Specificity of the DNA probe: the Gibbs free energy of non-matching duplexes is not zero!

Fluorescent Labeling of DNA



DNA targets are specific detected by Secondary DNA-probes with Fluorescent Labels

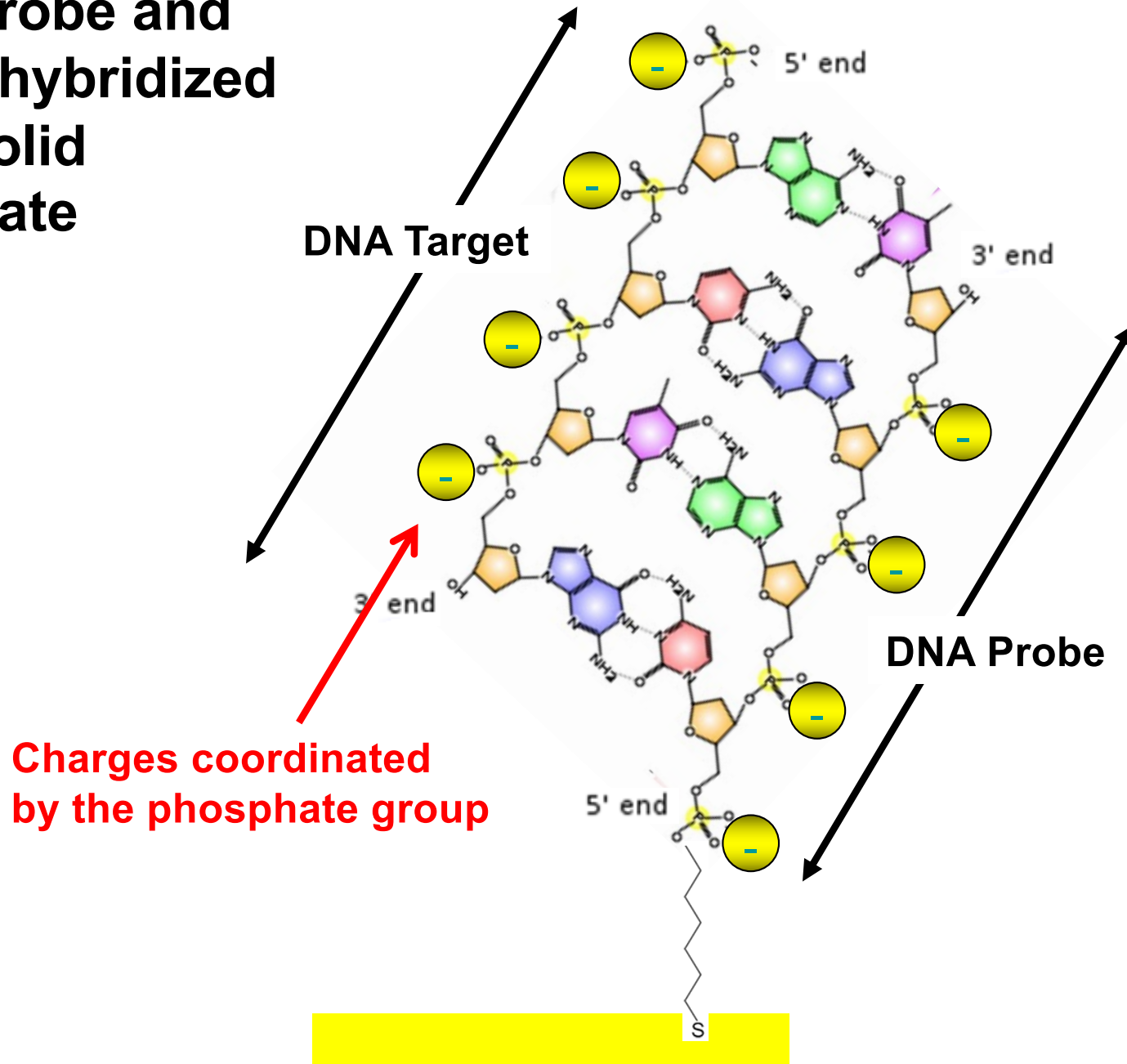
Amperometric Labeling of DNA



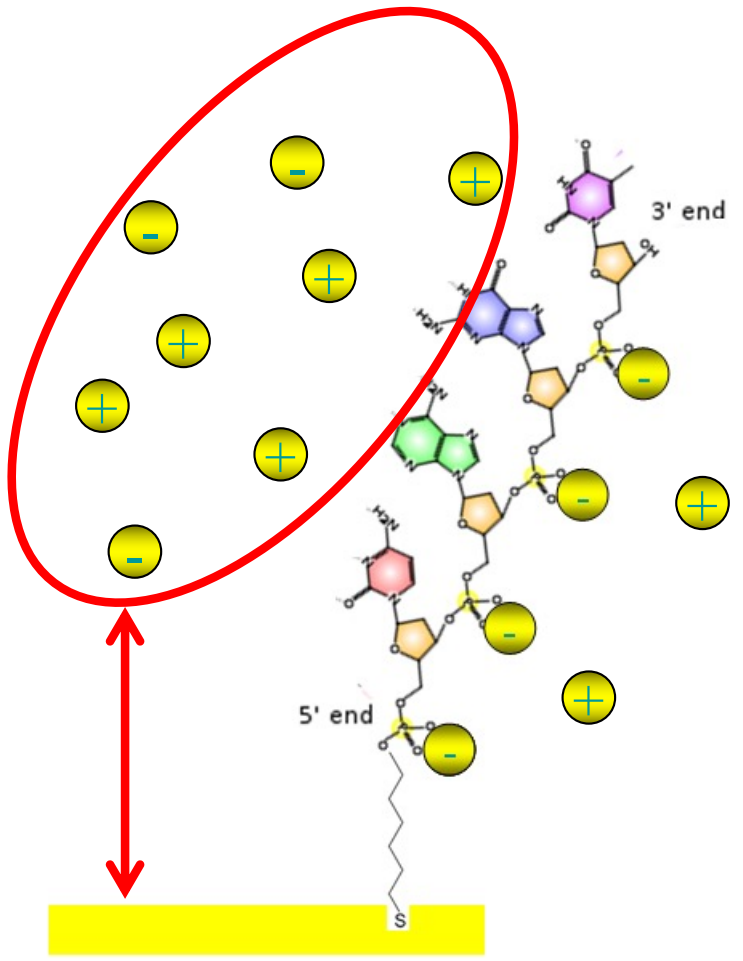
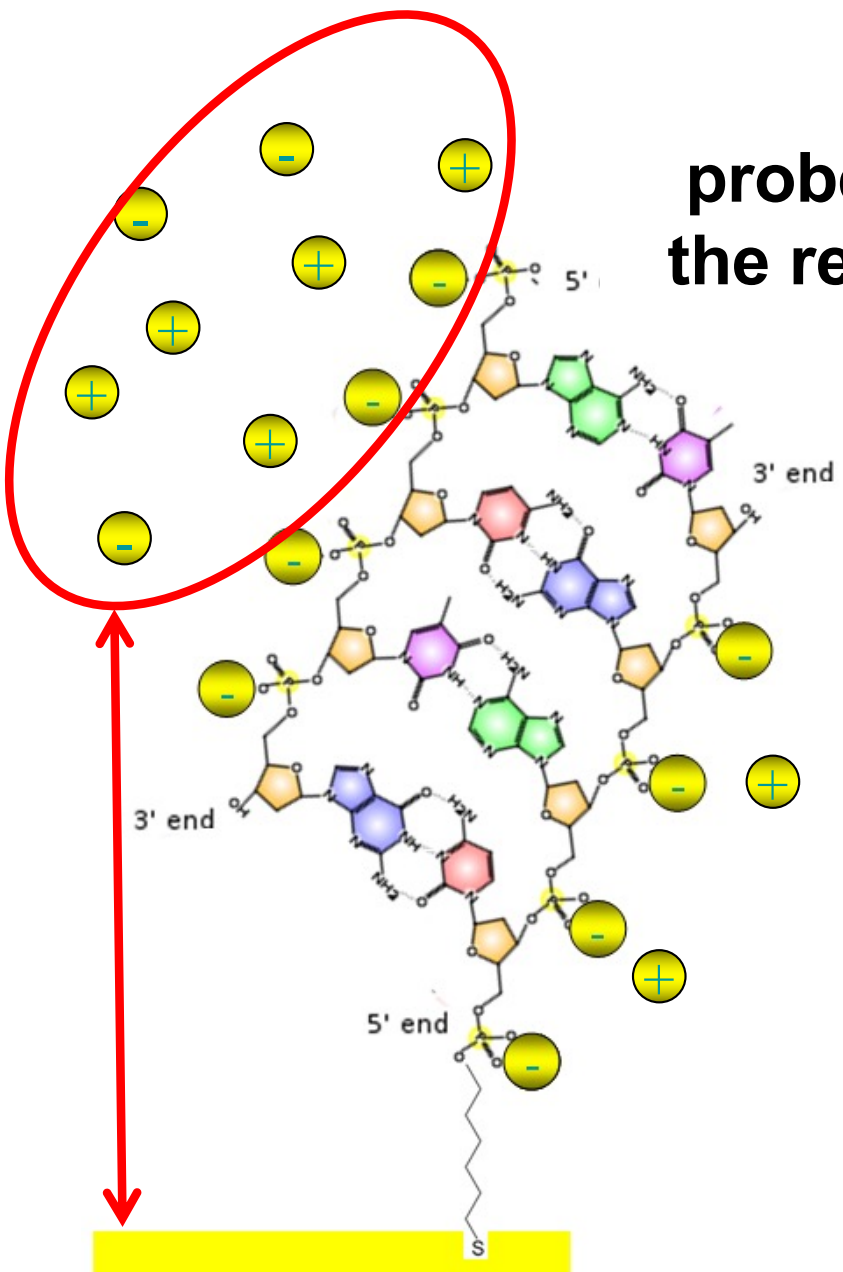
How it works:

- ✓ First, single stranded DNA molecules (about 20 bases) are immobilized by using a spotting machine on top of the gold electrodes due to gold-thiol coupling.
- ✓ Then, the chip is flooded with an analyte containing labeled target DNA ss: hybridization takes place in case of matching.
- ✓ A suitable substrate is applied to the buffer solution and it is enzymatically cleaved by the label.
- ✓ Resulting species starts an electrochemical redox process at the electrodes.
- ✓ Faradaic currents generated by the related redox process is detected and transduces DNA hybridization

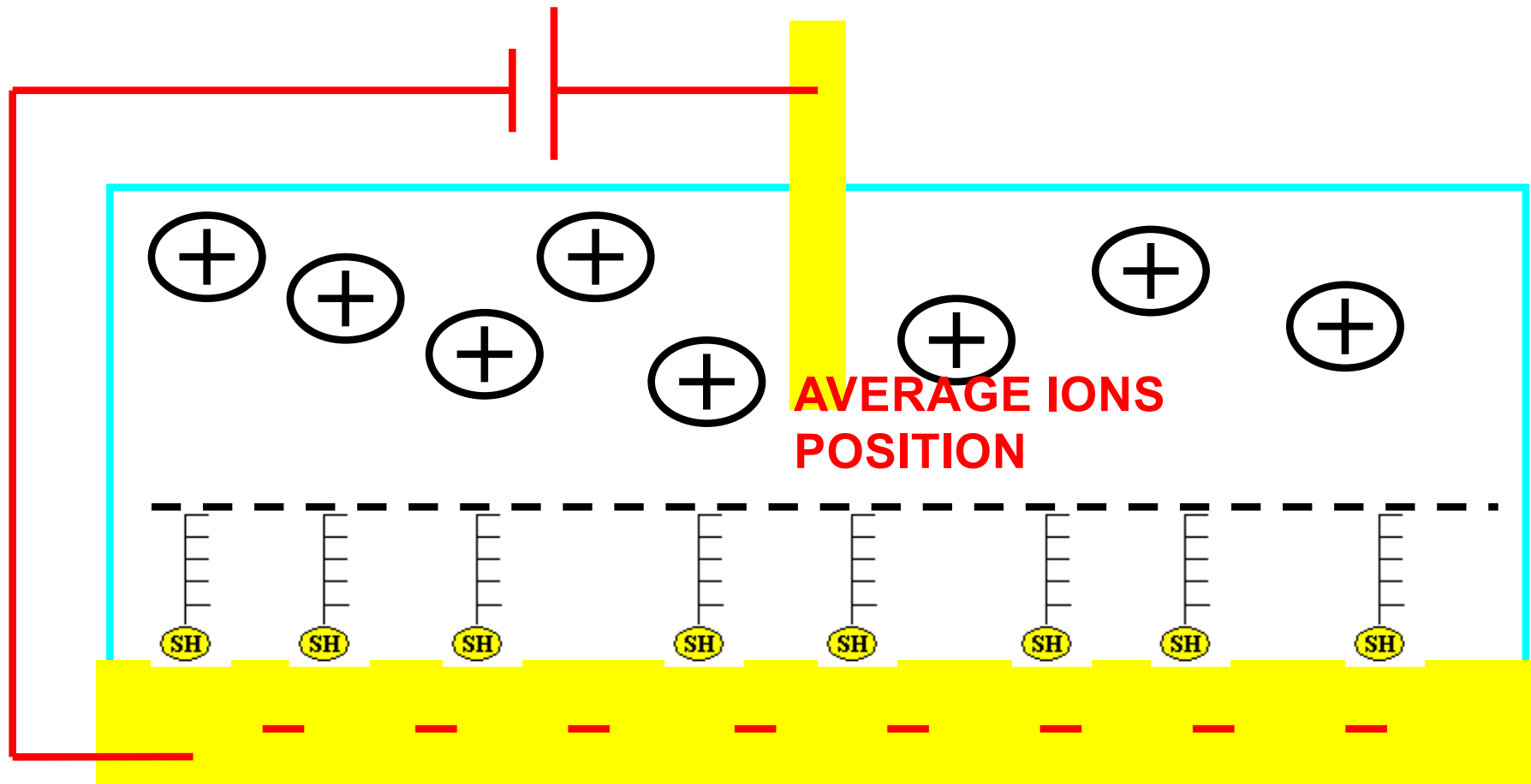
DNA probe and target hybridized on a solid substrate



DNA probe and hybridized probe/target on a solid substrate and the related solution ions distributions

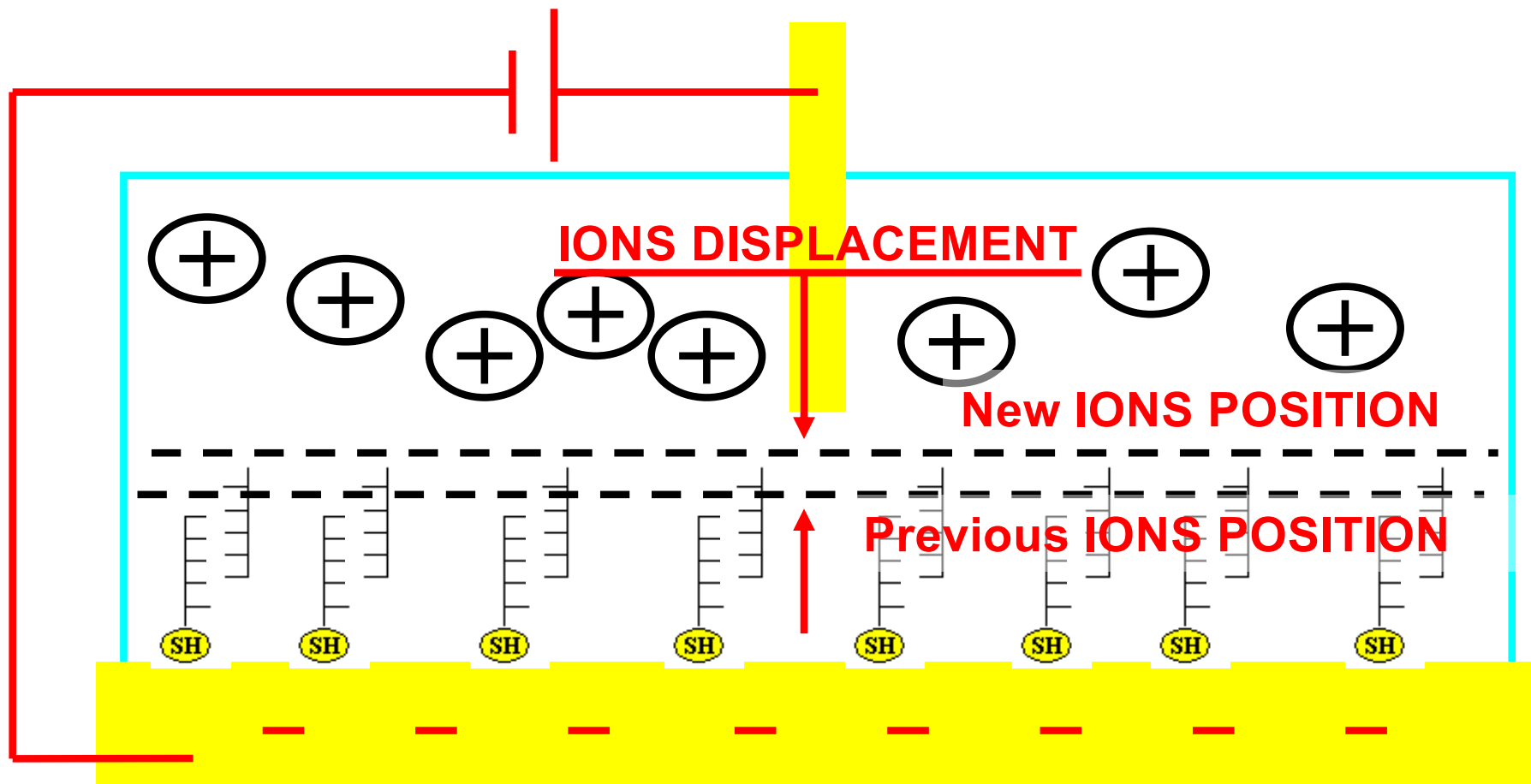


Electrochemical Interface



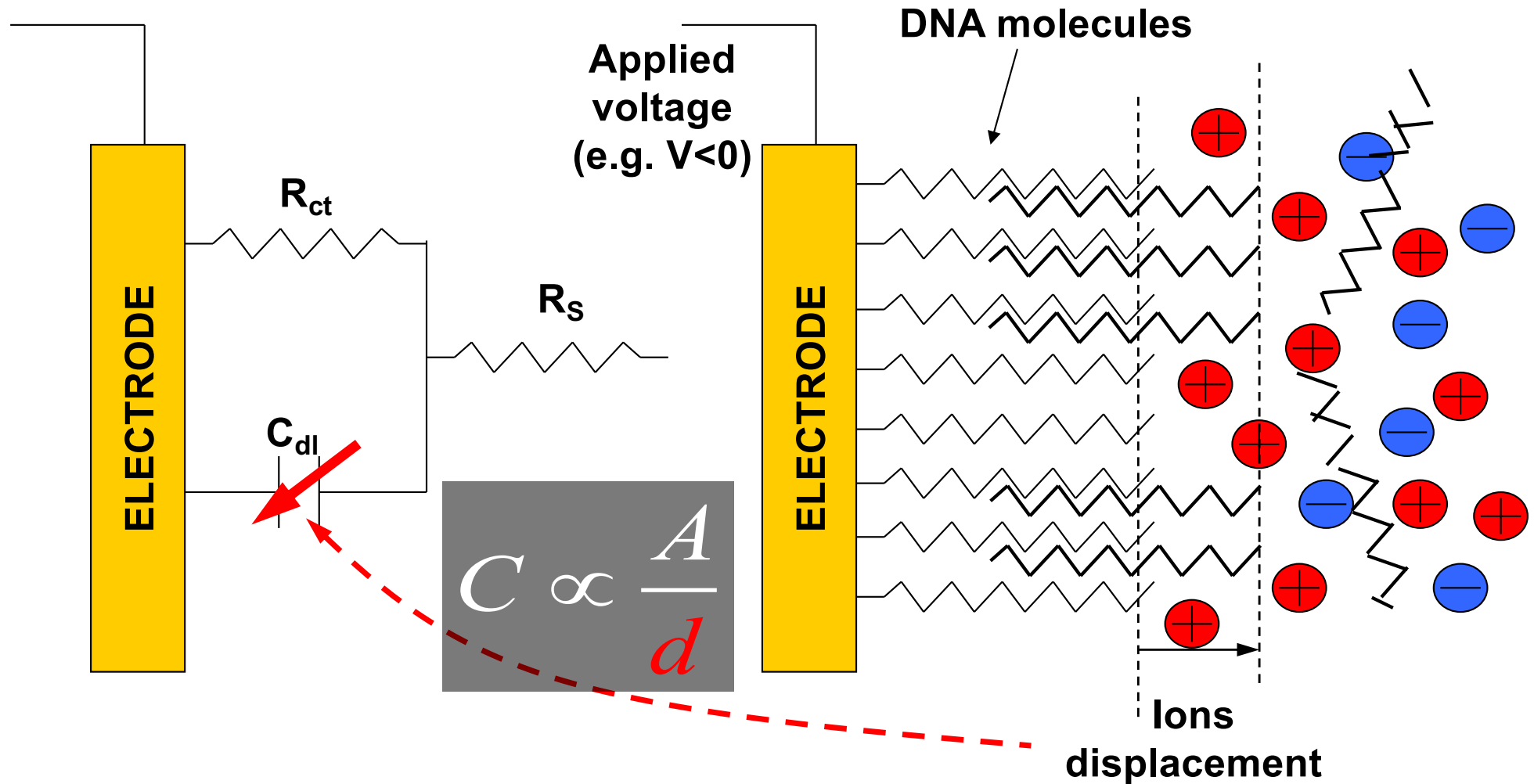
Ion planes are formed at the interface when electrodes immersed in solution are polarized

Electrochemical Interface



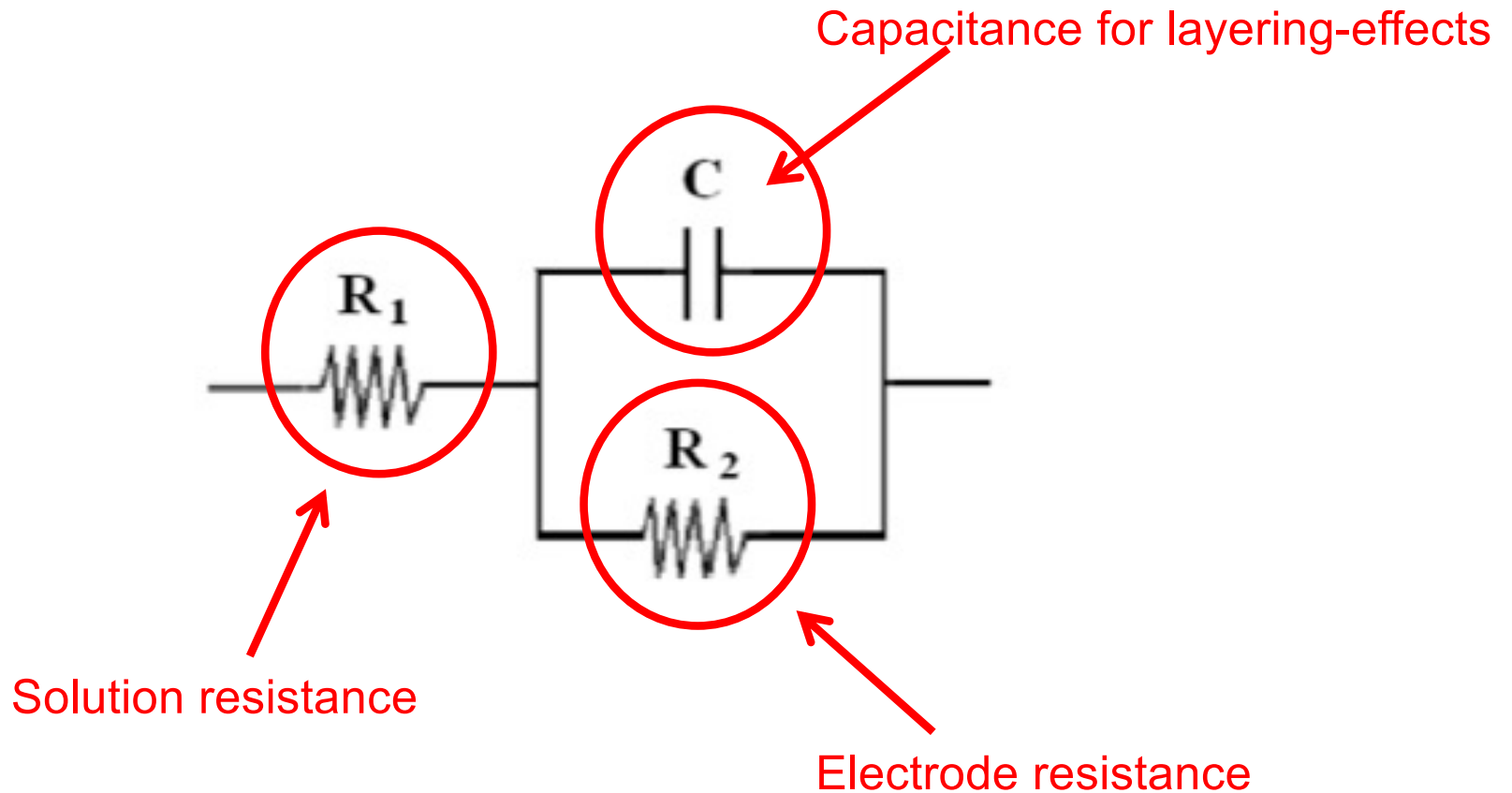
Ion planes are formed at the interface when electrodes immersed in solution are polarized

The Capacitance DNA Detection



Unlabeled ssDNA may be detected with capacitance measurements as due to charge displacement

Equivalent Circuit with Layering effects (Randle Model)





Q10

Does the resistance of a Resistor change with the frequency?

- A. Yes, of course!
- B. Yes, depending by the applied potential
- C. May be, depending by the type of the resistor
- D. No, if the applied potential is in D.C.
- E. Not at all



Q11

Does the impedance of a Resistor change with the frequency?

- A. Yes, of course!
- B. Yes, depending by the applied potential
- C. May be, depending by the type of the resistor
- D. No, if the applied potential is in D.C.
- E. Not at all**



Q12

Does the impedance of a Capacitor change with the frequency?

- A. Yes, of course!
- B. Yes, depending by the applied potential
- C. May be, depending by the type of the capacitor
- D. No, if the applied potential is in D.C.
- E. Not at all



Q13

Does the capacitance of a Capacitor change with the frequency?

- A. Yes, of course!
- B. Yes, depending by the applied potential
- C. May be, depending by the type of the resistor
- D. No, if the applied potential is in D.C.
- E. Not at all

Equivalent C of sensing electrodes

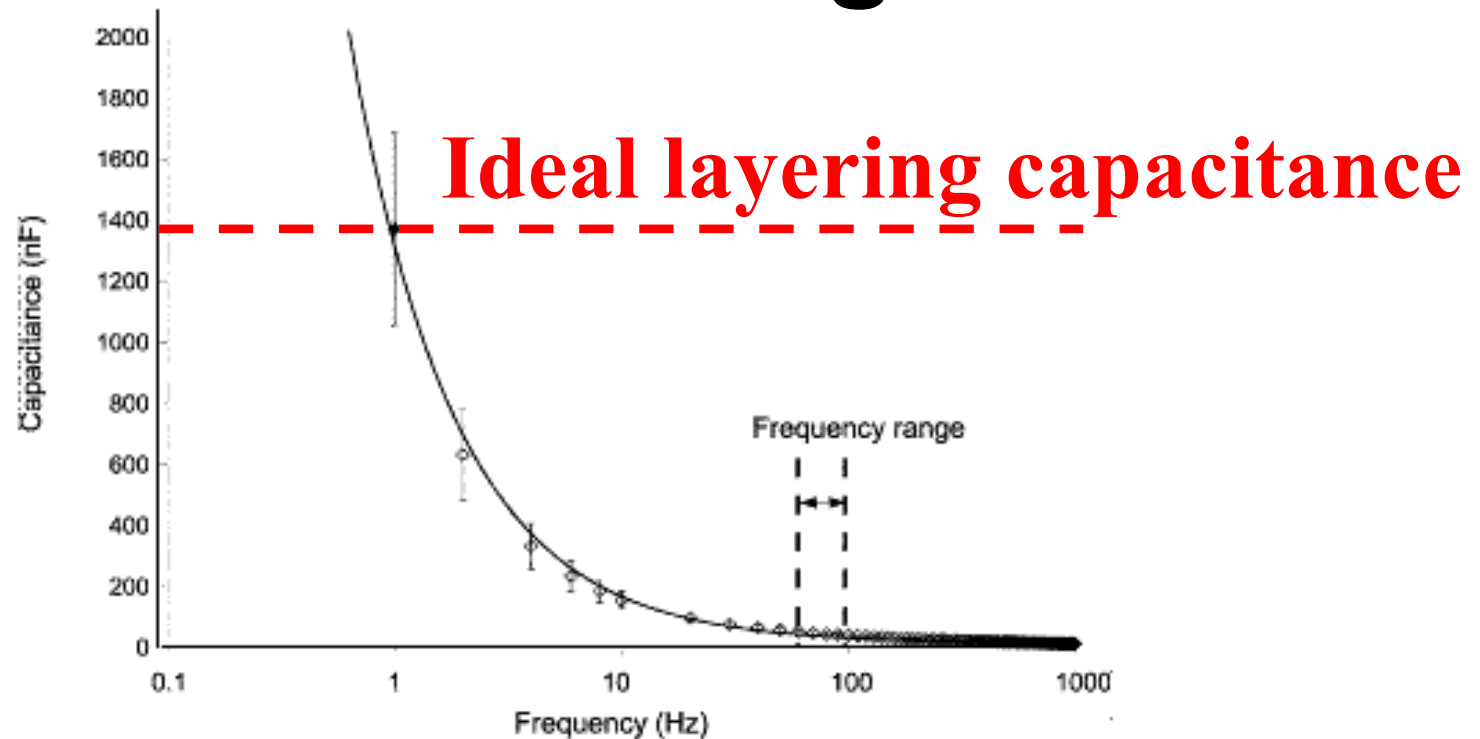
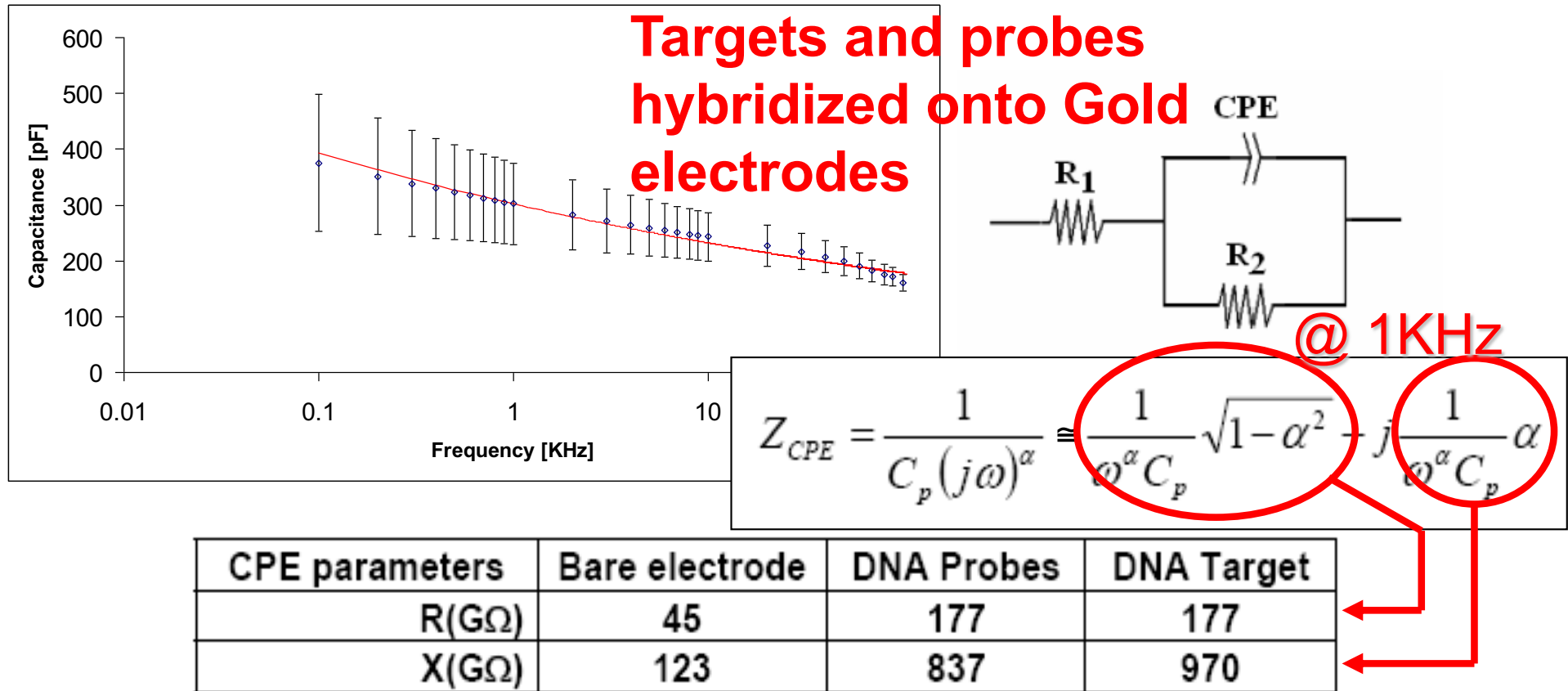


Fig. 9. Measured capacitance versus charge/discharge frequency on clean gold electrodes. The continuous line shows the fitting.

STAGNI *et al.*: FULLY ELECTRONIC LABEL-FREE DNA SENSOR CHIP IEEE SENSORS JOURNAL, VOL. 7, NO. 4, APRIL 2007

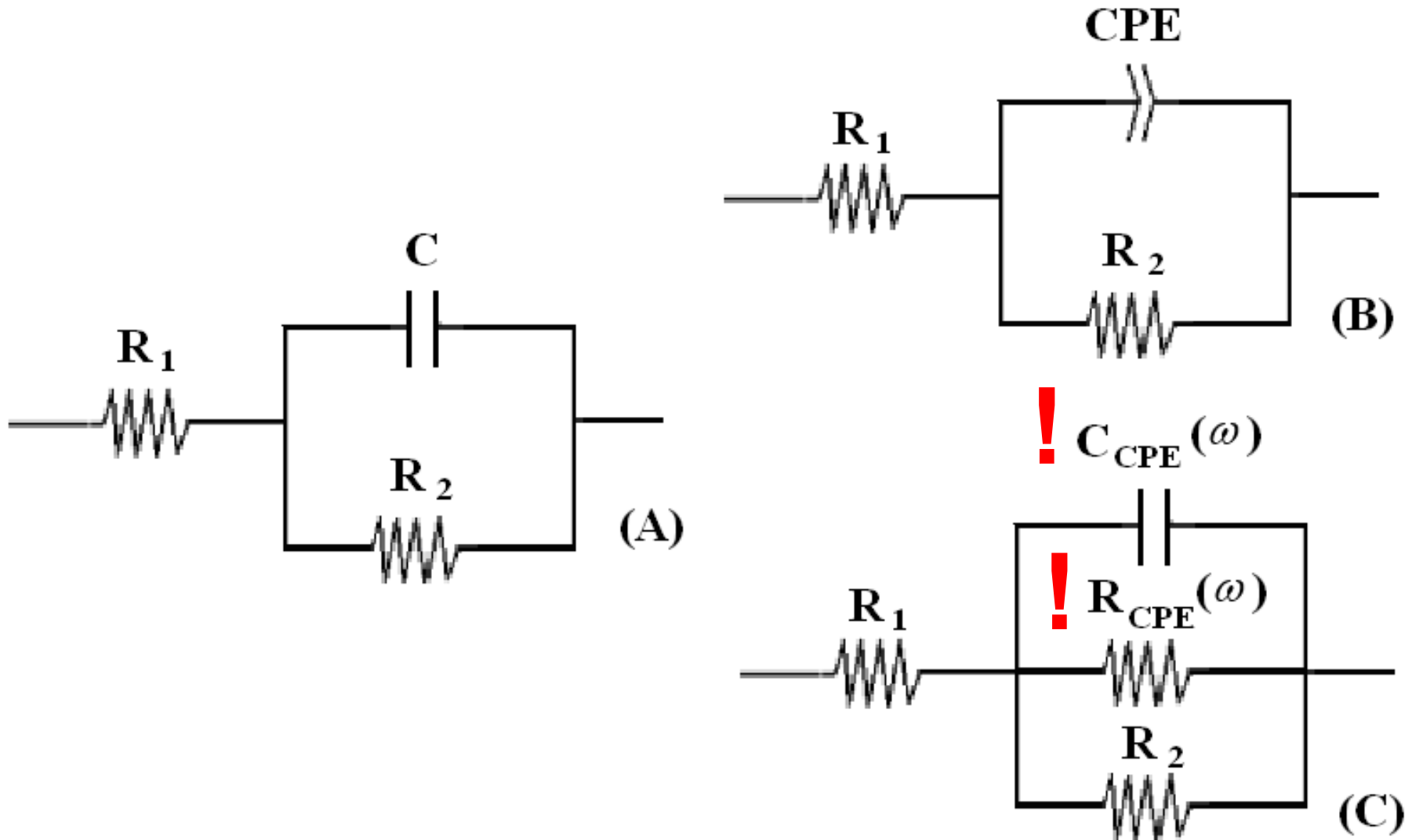
The equivalent capacitance of Helmholtz ion planes on bare electrodes is frequency-dependent

Equivalent C of DNA electrodes



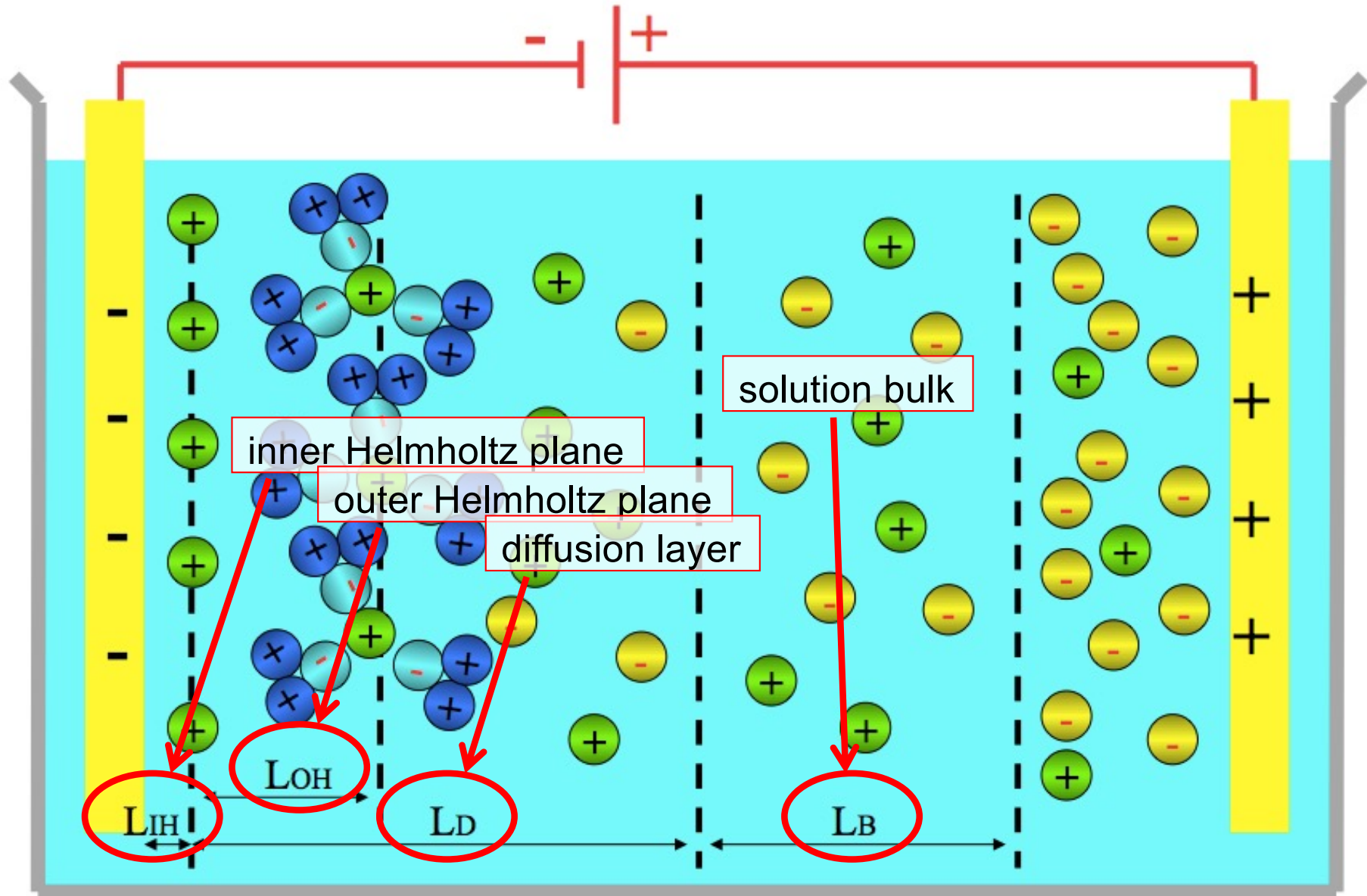
Charge transfer pathways through the DNA layer affect the ideal Capacitance behavior of the interface with the solution sample

Equivalent circuits



Equivalent circuits of DNA Bio/CMOS interface

Helmholtz Planes



Debye Length

Charge density: $\rho_e = \sum_i z_i e n_i$

z_i = charge of species i (e.g. +2, -1, etc.)

n_i = concentration of species i (number per volume)

$$\nabla f = \frac{\partial f}{\partial x} \hat{\mathbf{x}} + \frac{\partial f}{\partial y} \hat{\mathbf{y}} + \frac{\partial f}{\partial z} \hat{\mathbf{z}}$$

$$\nabla \cdot \nabla f = \nabla^2 f$$

$$\nabla^2 \phi = 0$$

In the bulk

$$\nabla^2 \phi = -\frac{\rho_e}{\kappa \epsilon_0}$$

Close to electrodes

For perturbation away from equilibrium at finite temperature

$$\hat{\phi} \equiv \phi - \phi_0$$

$$\rho_e = \sum_i z_i e n_{i0} \exp\left(-\frac{z_i e \hat{\phi}}{k_B T}\right)$$

Debye Length

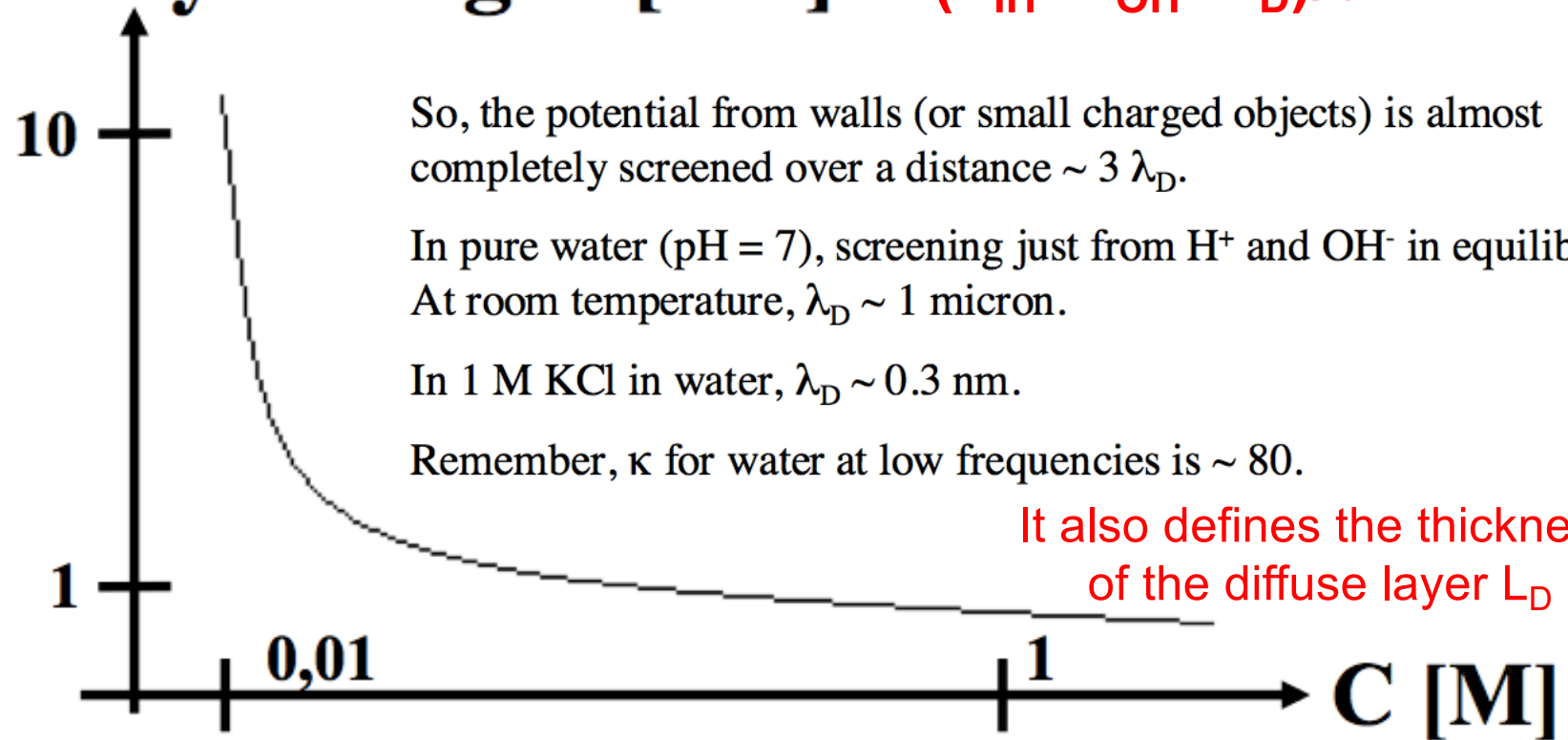
$$\nabla^2 \hat{\phi} = -\frac{1}{\kappa\epsilon_0} \sum_i z_i e n_{i0} \exp\left(-\frac{z_i e \hat{\phi}}{k_B T}\right) \approx -\frac{1}{\kappa\epsilon_0} \cancel{\sum_i z_i e n_{i0}} + \frac{e^2}{\kappa\epsilon_0 k_B T} \sum_i z_i^2 n_{i0} \hat{\phi} \equiv \frac{1}{\lambda_D^2} \hat{\phi}$$

~ 0 for equilibrium neutrality

$$\lambda_D \equiv \left(\frac{e^2}{\kappa\epsilon_0 k_B T} \sum_i z_i^2 n_{i0} \right)^{-1/2}$$

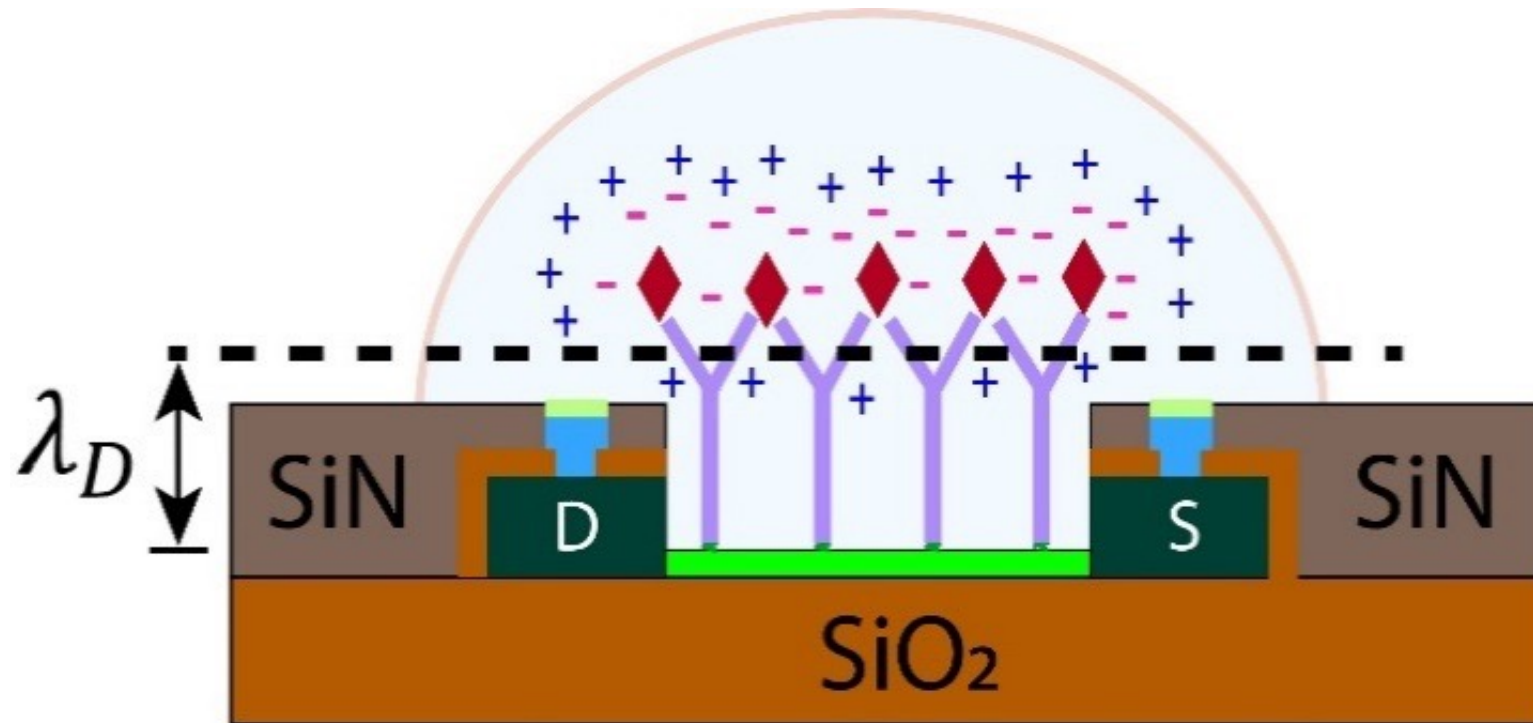
Debye Length

$$\text{Debye Length [nm]} = (L_{\text{H}^+} + L_{\text{OH}^-} + L_{\text{D}}) / 3$$



The Debye Length is defined as the region of charge carrier's net electrostatic effect in solution

Capacitance Detection & Debye Length



In liquid electrical detection

The Debye Length is top important to establish the limits of charge-based detections in solution